

31st Annual CIRMS Meeting

# Efficient image-guided rodent irradiations on high-throughput eFLASH platforms

KEVIN E. BYRNE, M.SC. MON, APR  $29^{TH}$ 



# Disclosures

I have no financial disclosures or conflicts of interest related to the content covered in this presentation.



### About me

Position:	Research Medical Physicist, Department of Radiation Oncology, UMSOM		
Location:	Medical School Teaching Facility (Office: 7-00E)		
Role:	Provide preclinical radiation physics and dosimetry support to the MCMP		
Primary Responsibilities:	Perform animal irradiations for MCMP studies and as a service to other investigators		
	Maintain QA program for irradiators and dosimeters		





### MCMP @ RadOnc @ UMSOM

The Medical Countermeasure Program (MCMP) advances the development of potential mitigators of acute radiation sickness (ARS) and delayed effects of acute radiation exposure (DEARE).

Internationally recognized for our expertise in MCM development studies in mouse, rabbit, pig, and NHP models.





# **UMSOM FLASH systems**

#### **UHDR electrons**

#### Varian Clinac 21-EX

Energy	16 MeV	
PRF	up to 180 Hz	
Nominal PW	5 µs	
DR <sub>average</sub>	up to ~130 Gy.s <sup>-1</sup>	
DR <sub>instant</sub>	up to 10 <sup>5</sup> Gy.s <sup>-1</sup>	
Duty Cycle	<0.1%	

#### **UHDR protons**

#### Varian ProBeam

Energy

250 MeV

DR<sub>average</sub>

up to ~120 Gy.s<sup>-1</sup>

#### Varied parameters:

PRF, Duty Cycle, PW, DR<sub>instant</sub> (10<sup>3</sup> Gy.s<sup>-1</sup>)



#### Linac-based eFLASH systems







### Matched UHDR and CONV beam at UMSOM



d<sub>max</sub> reduced from 3.4 to 0.5 cm 96% until 2 cm

### **eFLASH** Platform





up to ~130 Gy.s<sup>-1</sup>

Off-axis distance (cm)



### **Sample Collimator Designs**



4 x HTLI (or 3 x WTLI) – 3 cm diameter

### **Collimator-Template Matching**



4 x HTLI (or 3 x WTLI) – 3 cm diameter



#### 5 x flank – 1 cm diameter





### **Positioning Templates**







# **UHDRe – Rat Prostate**





Collimated beam profiles obtained at conventional (CONV) and ultrahigh (FLASH) dose rates. The 80%-20% penumbra increases from 0.035 cm at the entrance (0 cm depth) to 0.87 cm at 3 cm depth. The PDD of the collimated UHDR beam remains above 88% up to 3 cm, the approximate anterior-posterior thickness of an adult rat.



# "Anatomy [...] of Rat Prostate"



Figure 1. Macroscopic appearance of rat prostate and other surrounding anatomical structures at 61 weeks of age. (A) In situ photography of an animal from control group, ventral view; (B) Photography of prostate from an induced animal (dorsal view). Seminal vesicles and coagulative glands extended caudally. (C) Line diagram of prostate, urinary bladder and closed sex glands. Coagulating glands (CG), dorsal (DP) and ventral prostate lobes (VP), seminal vesicles (SV) and urinary bladder (UB).



### **Electron FLASH: Rat Prostate**





CBCT images showing adequate contrast for lower abdominal soft tissue visualization in the axial (A) and sagittal (B) views of a Copenhagen rat.



2D kV planar image highlighting the location of a CT dot (red circle) and the scintillator tip (green rectangle).



### **Positioning Templates**





Byrne et al (2024) doi.org/10.1002/mp.16909



#### Reason #2 – UHDR Setup

It takes time to leave service mode, image, re-position, re-enter service mode

<u>AND</u>



Beam stability measurements. (a) FLASH beam ramp-up on 3 separate days. (b) FLASH beam repeatability on 3 separate days. (c) FLASH beam reproducibility over 7 days.



### X-RAD 320 (PXi)

Up to 320 kVp (relatively high)

Static x-ray tube (robust, few moving parts)

Broad beam (fits more animals, high throughput)

Classic muscle car: "fast and simple"



X-PLATE INTO

### Small Animal Radiation Research Platform (SARRP, Xstrahl)

Rotating X-Ray tube, couch motion (x, y, z, yaw)

Up to 225 kVp (intermediate)

CBCT (gantry at 90, couch rotates)

**MuriPlan TPS** 

Crossover SUV: "versatile and practical"



$$Total (\$) = 200 \ mice \ \times 10 \ \frac{fractions}{mouse} \ \times 0.25 \ \frac{hours}{fraction} \ \times 240 \ \frac{\$}{hour} \ \times 75\% =$$



### High-throughput platform for the X-RADs



AGFA DR14s Wireless Digital Radiography Panel

Beam	SARRP	X-RAD 320 F1	X-RAD 320 F2
Peak Energy (kVp)	225	320	320
Filtration	0.15 mm Cu	2 mm Al	0.75 mm Sn + 1.5 Al + 0.25 Cu
Mean Energy* (keV)	~80	~90	~160
HVL	0.6 mm Cu	1.0 mm Cu	3.8 mm Cu

### Solution: High-throughput collimator for the X-RAD







#### **Reason #3 – Workflow Parallelization (CONV kV example)**





### "Banking" into place conserves positioning





Through collimator



Through Positioning Plate only



# **Characterization: Profiles and E2E**





### Proton FLASH example: Hemi-thorax





Mossahebi et al (in review)



# Take home points

- 1. SAI throughput can be improved, without adversely affecting accuracy, by using customized collimator templates and image guidance
- 2. Parallelization of the workflow improves efficiency and is especially useful in FLASH experiments involving collimators, where wait times are required between runs due to activation.

#### References



Mott JHL, West NS. Essentials of Depth Dose Calculations for Clinical Oncologists. Clin Oncol. 2021;33(1):5-11. doi:10.1016/j.clon.2020.06.021

Berne A, Petersson K, Tullis IDC, Newman RG, Vojnovic B. Monitoring electron energies during FLASH irradiations. Phys Med Biol. 2021;66(4). doi:10.1088/1361-6560/abd672

Xie DH, Li YC, Ma S, et al. Electron ultra-high dose rate FLASH irradiation study using a clinical linac: Linac modification, dosimetry, and radiobiological outcome. Med Phys. 2022;49(10):6728-6738. doi:10.1002/mp.15920

Garty G, Obaid R, Deoli N, et al. Ultra-high dose rate FLASH irradiator at the radiological research accelerator facility. Sci Rep. 2022;12(1). doi:10.1038/s41598-022-19211-7

Lempart M, Blad B, Adrian G, et al. Modifying a clinical linear accelerator for delivery of ultra-high dose rate irradiation. Radiotherapy and Oncology. 2019;139:40-45. doi:10.1016/j.radonc.2019.01.031

Rahman M, Ashraf MR, Zhang R, et al. Electron FLASH Delivery at Treatment Room Isocenter for Efficient Reversible Conversion of a Clinical LINAC. Int J Radiat Oncol Biol Phys. 2021;110(3):872-882. doi:10.1016/j.ijrobp.2021.01.011

Szpala S, Huang V, Zhao Y, et al. Dosimetry with a clinical linac adapted to FLASH electron beams. J Appl Clin Med Phys. 2021;22(6):50-59. doi:https://doi.org/10.1002/acm2.13270

Poirier Y, Mossahebi S, Becker SJ, et al. Radiation shielding and safety implications following linac conversion to an electron FLASH-RT unit. Med Phys. 2021;48(9):5396-5405. doi:10.1002/mp.15105

Schüler E, Trovati S, King G, et al. Experimental Platform for Ultra-high Dose Rate FLASH Irradiation of Small Animals Using a Clinical Linear Accelerator. Int J Radiat Oncol Biol Phys. 2017;97(1):195-203. doi:10.1016/j.ijrobp.2016.09.018

Byrne KE, Poirier Y, Xu J, et al. Technical note: A small animal irradiation platform for investigating the dependence of the FLASH effect on electron beam parameters. *Med Phys.* 2024;51(2):1421-1432. doi:10.1002/mp.16909

Poludniowski G, Landry G, Deblois F, Evans PM, Verhaegen F. SpekCalc: A program to calculate photon spectra from tungsten anode x-ray tubes. Phys Med Biol. 2009;54(19). doi:10.1088/0031-9155/54/19/N01



# **THANK YOU!**

#### **Acknowledgments:**

Dr. Kai Jiang

Dr. Sina Mossahebi

Binny Bhandary, MS

Dr. Yannick Poirier

Dr. Amit Sawant

Dr. Erika Davies