Dose measurements in radiobiology x-ray irradiators



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in vitro cell studies



in vivo animal studies



Understanding of disease, human treatment

Simplified goal: correlate delivered dose to biological endpoint



- "Cabinet irradiators"
- High-throughput cell or animal studies
- Mounted X-ray tube
 - 160-360 kVp
 - Variable filtration
 - Stated dose rate 1-15 Gy/min
- This will focus on XRad 320



Precision X-Ray, Inc



- Ability to intercompare results requires accuracy in the stated doses that is at least equal to the precision of the measurements¹
- Reproducibility concerns
 - Drug-radiation combination studies not reproducible²
 - Spot-check in phantom average 10% dose discrepancy³
- Lack of reporting^{1,3}

- 1. M. Derosiers et al, J Res Natl Inst Stand Technol, 118, 2013
- 2. H. Stone et al, Transl Oncol, 9, 2016
- 3. Pedersen et al, Rad Res, 185, 2016



- Requirement of increased irradiation detail reporting and NISTtraceable dosimetry
 - Enforce standards for reproducible, translational studies
- For clinical orthovoltage x-rays AAPM TG-61 protocol
 - Limited distance, cabinet shielding, field size changes
- Requires characterization of the x-ray spectrum
 - However, these radbio irradiators are unlike any NIST or ISO beams



University of Wisconsin Accredited Dosimetry Calibration Lab (UWADCL)

	Beam Code	Added Filter (mm Al or Cu)	HVL1 (mm Al)	HVL1 (mm Cu)	HC (percent)	Air Kerma Rate (mGy/sec)	
XRa • • Wh	ad 320 : 320 kVp 1 or 4 mm C at beam is aj "sha user	Cu HVL ("F1" or "F ppropriate? all be calibrated a 's beam quality in	2") t a beam terms of	quality suf both the t	ficiently c ube poter	lose to the itial and HVL"	
	UW120-M	3.0 Al + 0.10 Cu	6.77		75	2.365	
	UW150-M	2.83 Al + 0.28 Cu	10.1	0.657	87	2.173	
	UW200-M	1.00 Al + 1.01 Cu	14.8	1.63	95	1.930	
	UW250-M	1.96 Al + 2.36 Cu	18.3	3.01	98	1.633	



- Spectrum affects dosimeters
- TG-61

$$D_{w,z=0} = MN_{K}B_{w}P_{\text{stem,air}}\left[\left(\frac{\mu_{\text{en}}}{\rho}\right)_{\text{air}}^{w}\right]_{\text{air}}$$

Dosimetry spot-checks require appropriate calibration beam





To characterize the XRad 320 and assess the effects of beam quality on detector response



- From nominal HVL alone: photon beams are different than reference
- Approximate XRad 320 spectra by matching HVL
 - Two filter packs generated
- Air kerma rate measured with A3 chamber
 - Allows for measurement in a known setup at UWMRRC



1. Tom Heaton, Secondary-Level Laboratories: Methodology for a Calibration Program

Simulation of RadBio Beams

- Simulate spectra from XRad 320
 - Use to simulate detectors in-phantom
- EGSnrc¹
 - Previously validated M-series -1.150x-ray beams²
 - Benchmarked with thin-window 3410 water tank
- Phase space below filters

- 1. I. Kawrakow and D. W. O. Rogers, "The EGSnrc Code System: Monte Carlo simulation of electron and photon transport", NRC Report PIRS-701 (2003)
- 2. M. Lawless, PhD Thesis, 2016







Detector Response in Mouse Phantom

1.5

1.4

1.3

1.2

1.1

1.0

0.9

elative response

- TLD energy response
 - Air vs water difference²
- Determine how beam quality affects TLD response in phantom
 - Energy corrections for spot-check measurements
- 3D-printed murinemorphic phantoms
 - CT image sets of 25 g lab mouse
 - TLD-100 microcubes in kapton
 - Resin composition measured and accounted for in simulation



100

average photon energy / keV

M(X)

1000

1

- 1. Nunn et al. Medical Physics, Vol.35 (5) 2008
- 2. Lawless, PhD Thesis, 2016



- TLDs simulated in phantom
- Electron spectra at 1.5 cm depth simulated
 - Compare M-series beams to RB beams



- Electron spectra at 1.5 cm depth simulated
 - Compare M-series beams to RadBio beams
- Electron spectra for RadBio beams similar to M-series



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- Dose to water, dose to TLD, air kerma simulated
 - Detailed simulation of irradiation geometry and NIST-matched air-kerma rates
 - M150-M250, ⁶⁰Co, RB Beams
- TLDs irradiated to the same dose in phantom at each energy
 - Detector output per dose to water

$$M(X) = \frac{\left(R/D_{\rm w}\right)_X}{\left(R/D_{\rm w}\right)_{\rm ref}}$$

Monte Carlo-predicted response

$$C_{\rm MC}(X) = \frac{\left(D_{\rm det}/D_{\rm w}\right)_X}{\left(D_{\rm det}/D_{\rm w}\right)_{\rm ref}}$$

Detector output/dose to TLD

$$\eta(X) = \frac{M(X)}{C_{\rm MC}(X)} = \frac{\left(R/D_{\rm det}\right)_X}{\left(R/D_{\rm det}\right)_{\rm ref}}$$

Pedersen et al 2015







- RadBio spectra compared to NIST-matched beams
 - Photon in-air and electron spectra at plane of TLDs
 - TLDs sensitive to spectrum at depth of measurement
- Measured and intrinsic detector responses of RadBio beams agreed with the reference beams within uncertainty
- With selection of appropriate reference beam, TLD microcube measurements in-phantom require minimal energy response corrections



- Cliff Hammer
- Dr. Mike Lawless
- UWMRRC students and staff
- Customers of the UWADCL, whose calibrations help to fund student research

Thank you for your attention