



# Alpha and Auger-Emitting Radionuclides for Therapy

Jonathan Engle

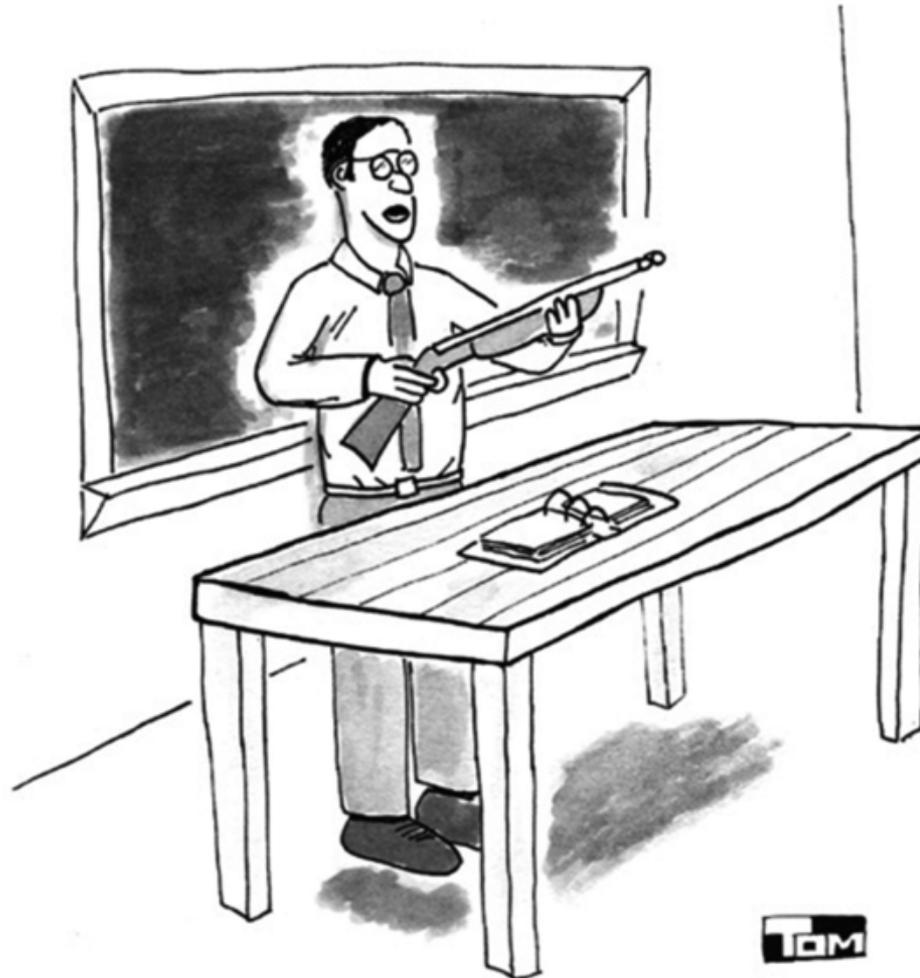
University of Wisconsin, Madison  
Department of Medical Physics

(& Recently: Los Alamos National Laboratory  
Chemistry Division  
Isotope, Inorganic, and Actinides Group)

CIRMS 2017  
Wednesday March 29



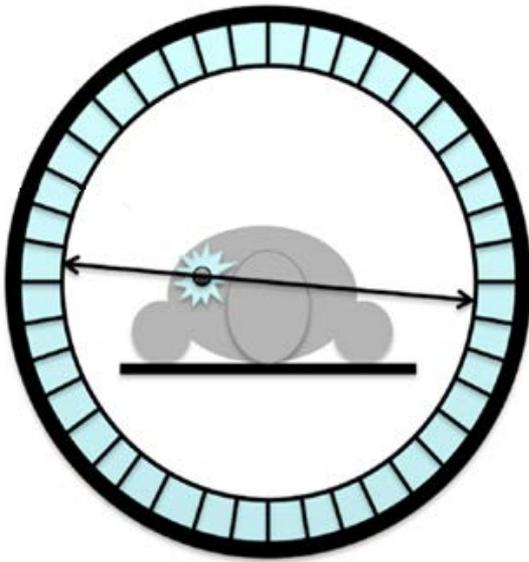
"PLEASE FEEL FREE TO INTERRUPT  
IF YOU HAVE A QUESTION."



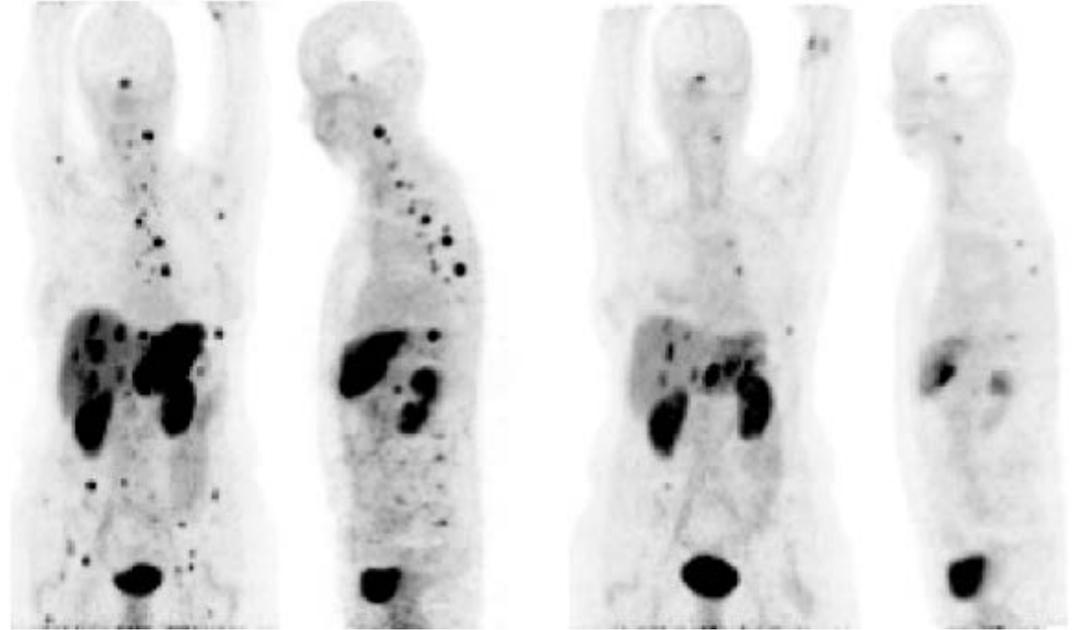
**TOM**



# Positron Emission Tomography



Van der Velt, et. al., Front. Oncol., 2013.

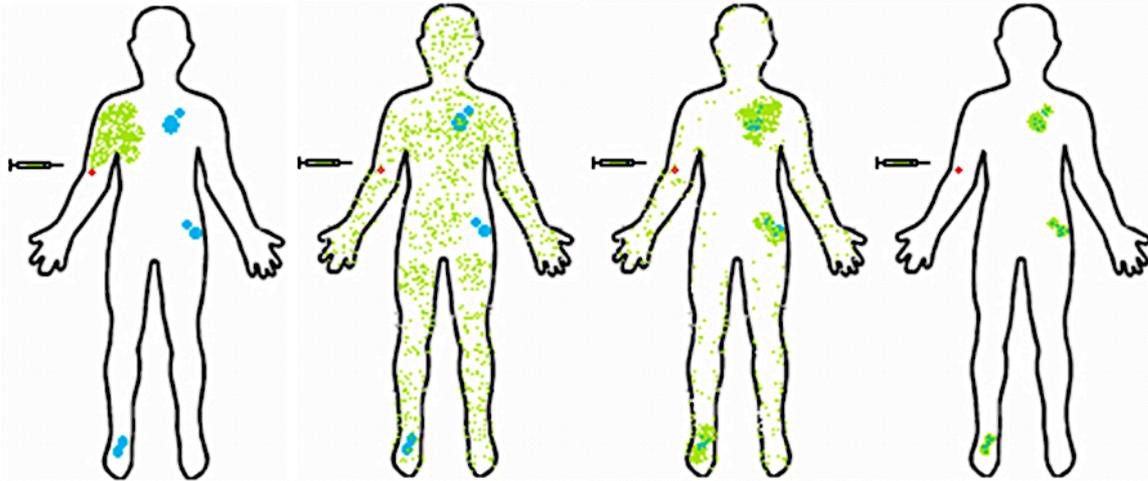


SNMMI Image of the Year, 2014. Molecular Imaging.

Isotope	Half-life ( $t_{1/2}$ )	$\beta^+$ Branch	$\beta^+$ Max Energy	Tracer examples
$^{11}\text{C}$	20.4 min	99.76%	0.96 MeV	PIB, Methionine, Choline
$^{13}\text{N}$	9.97 min	100%	1.19 MeV	Ammonia ( $^{13}\text{NH}_3$ )
$^{15}\text{O}$	2.04 min	99.89%	1.72 MeV	Water ( $^{15}\text{OH}_2$ )
$^{18}\text{F}$	109 min	96.9%	0.64 MeV	FDG, Fluoride ( $^{18}\text{F}^-$ )
$^{82}\text{Rb}$	1.27 min	96%	3.35 MeV	$^{82}\text{RbCl}$



# One Future for Radionuclide Production

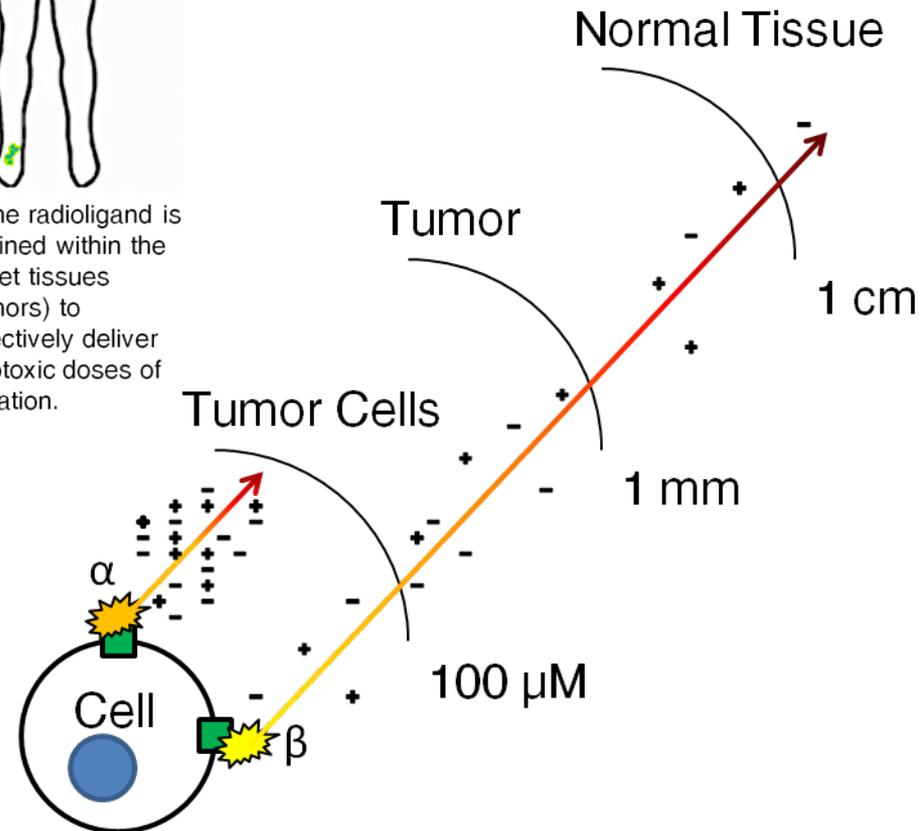


1. The targeted radioligand is administered systemically to the patient.

2. The radioligand distributes throughout the patient.

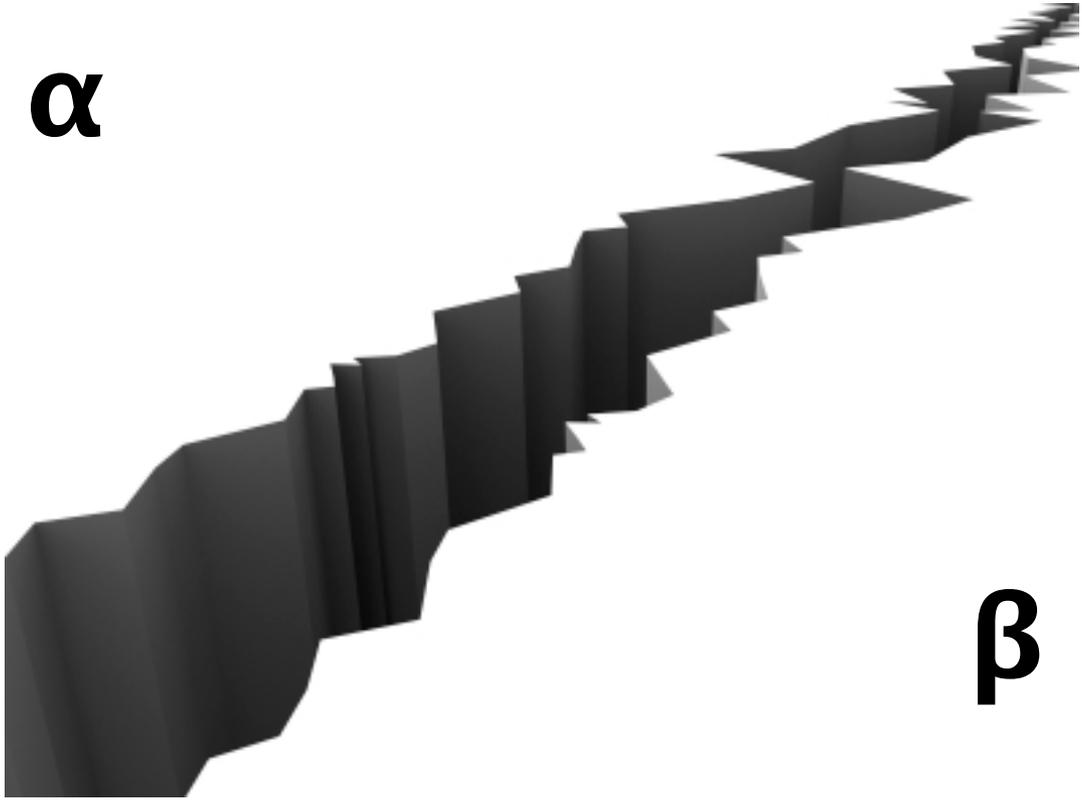
3. The radioligand localizes and concentrates in target tissues (e.g. tumors) reducing radiation dose to non-target normal tissues.

4. The radioligand is retained within the target tissues (tumors) to selectively deliver cytotoxic doses of radiation.





$\alpha$



$\beta$

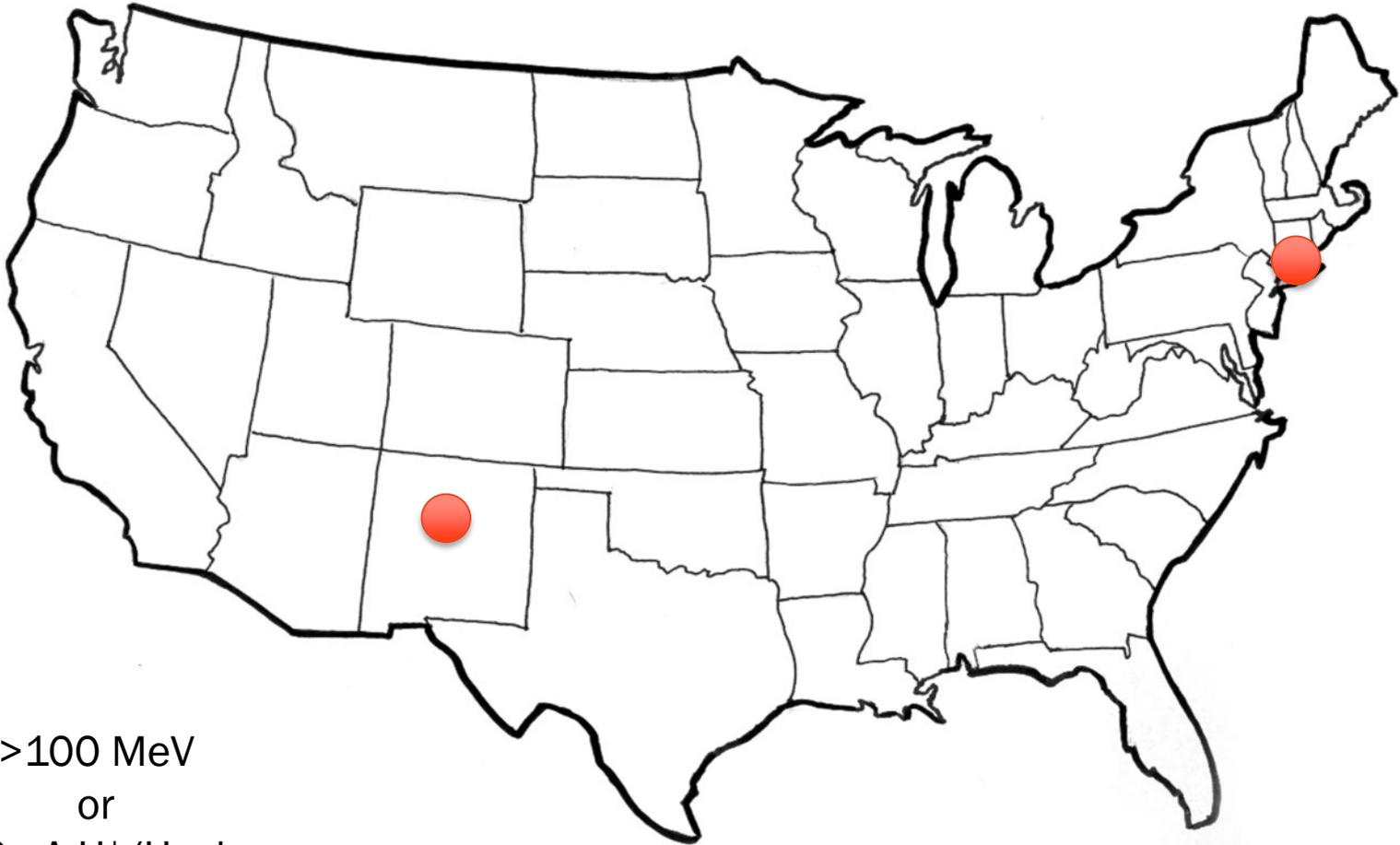


# How you take your coffee





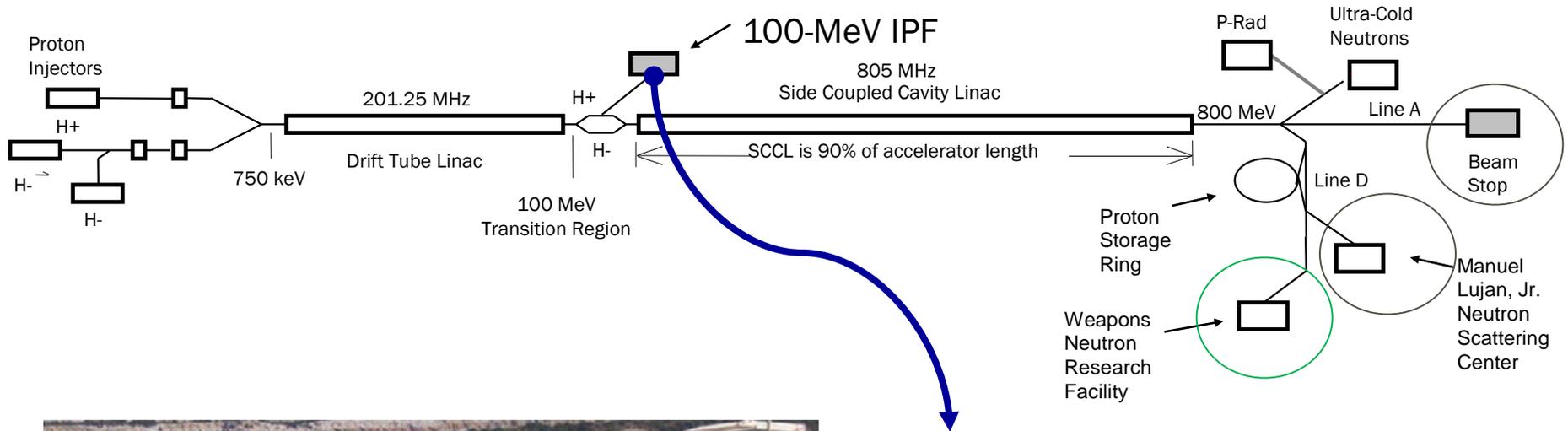
# National-Scale Facilities for Charged-Particle Irradiations and Radionuclide Production



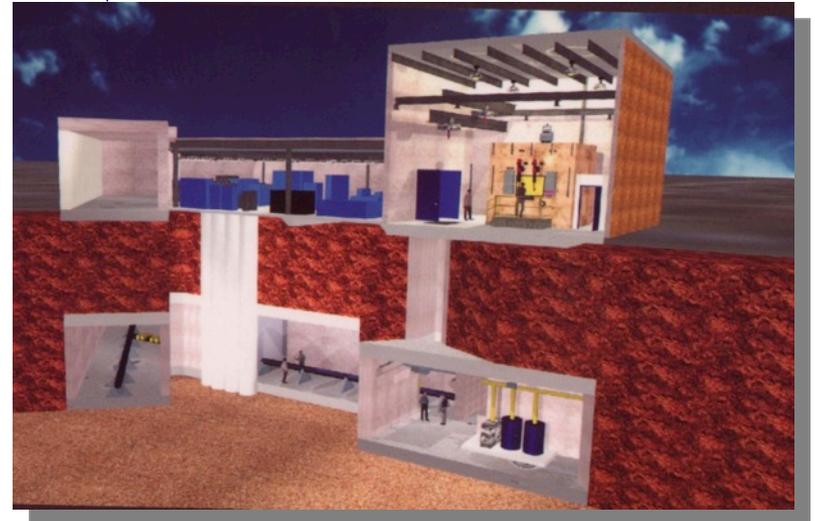
>100 MeV  
or  
>200  $\mu\text{A}$   $\text{H}^+/\text{H}^-$ ,  $\alpha$



# National Scale, Multi-User Infrastructure

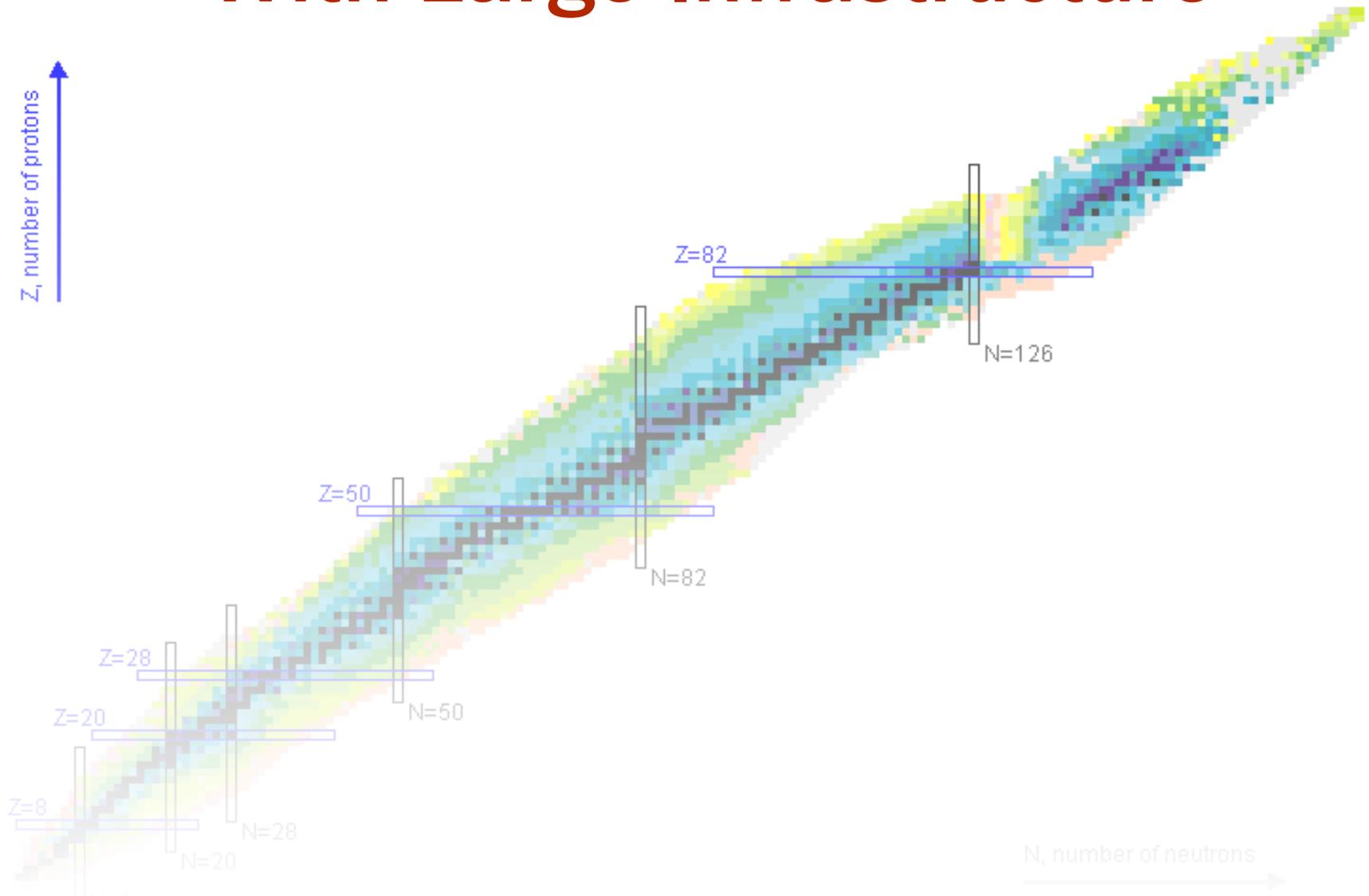


IPF at LANSCE



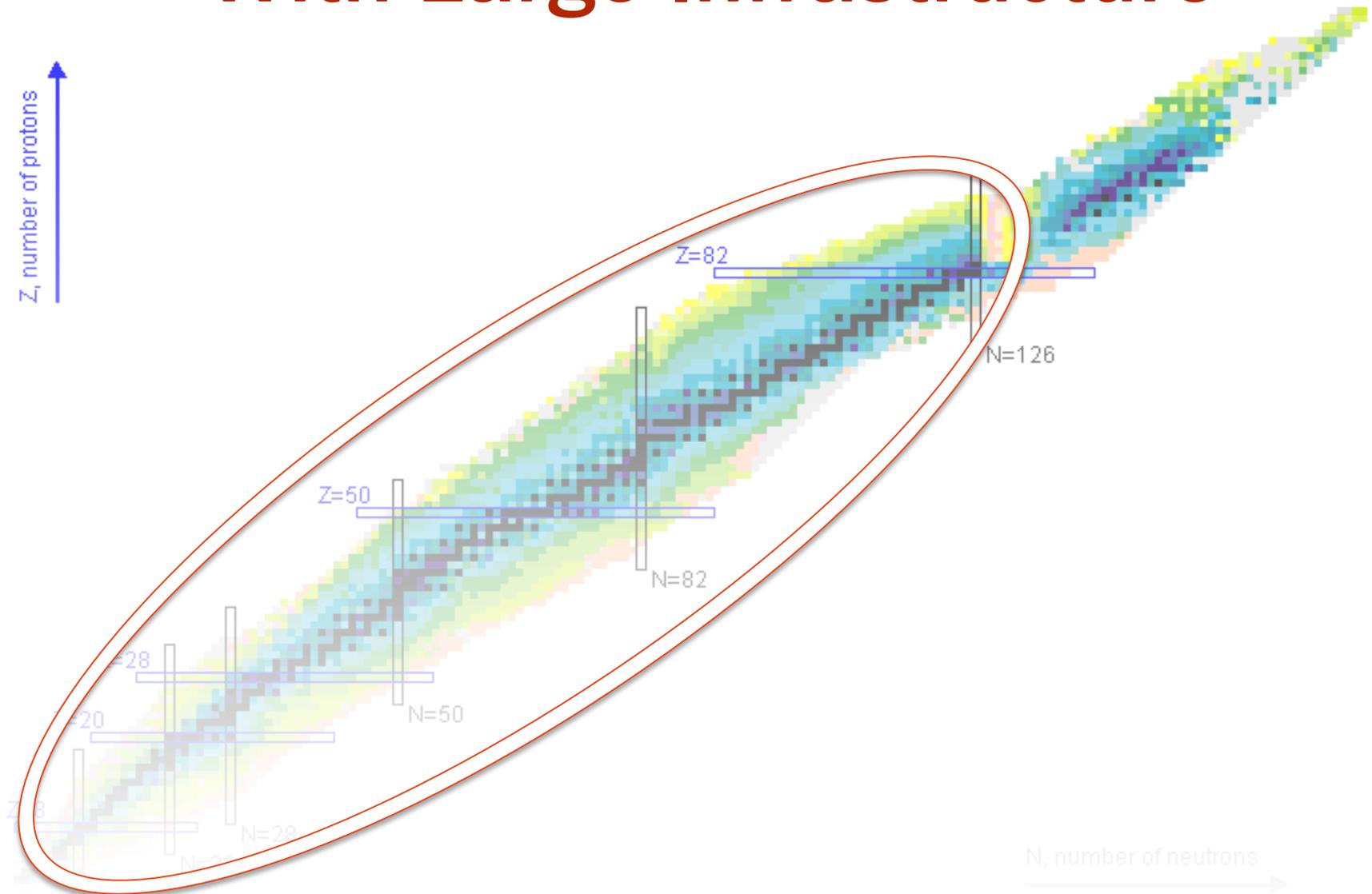


# With Large Infrastructure



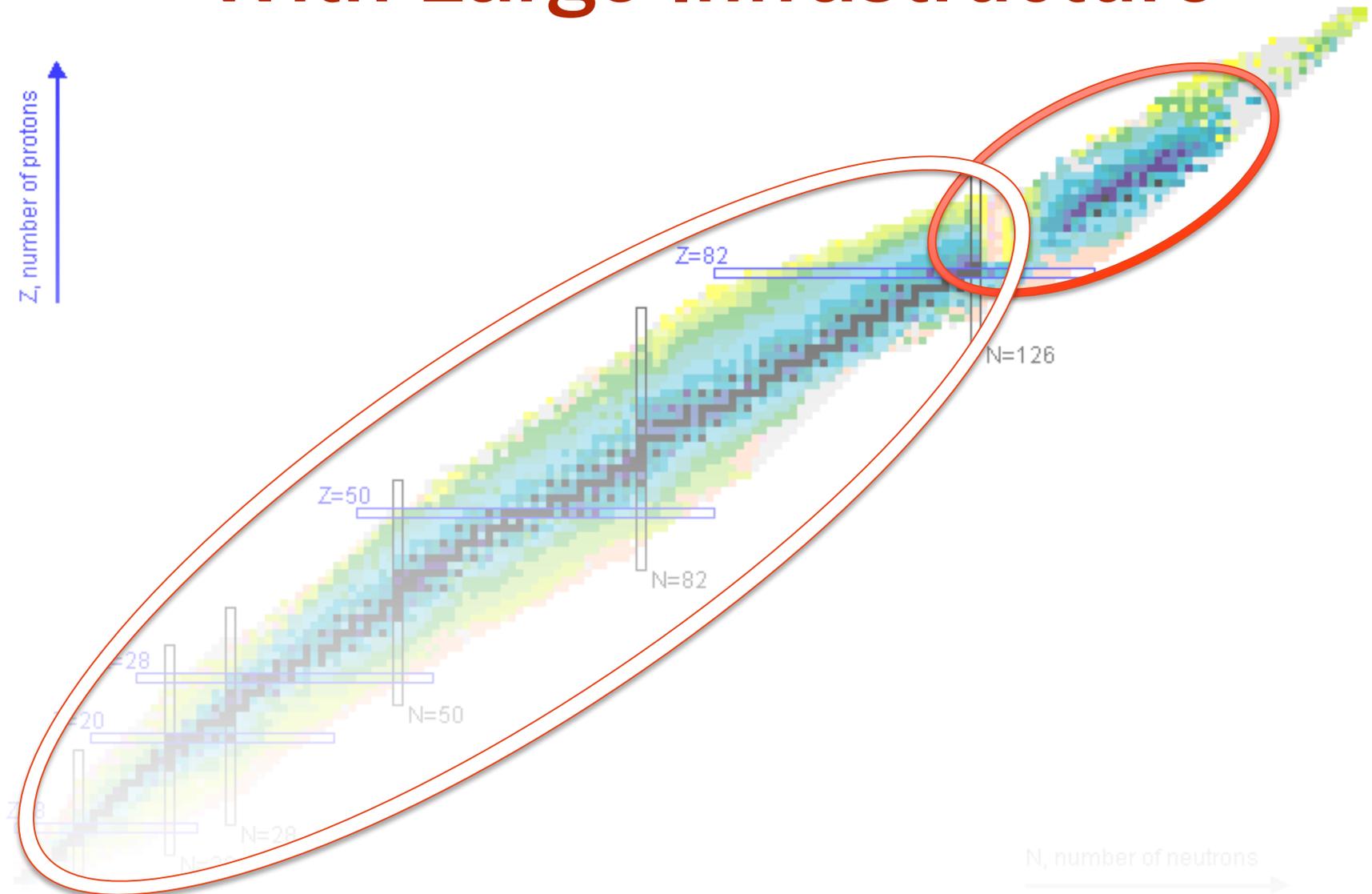


# With Large Infrastructure





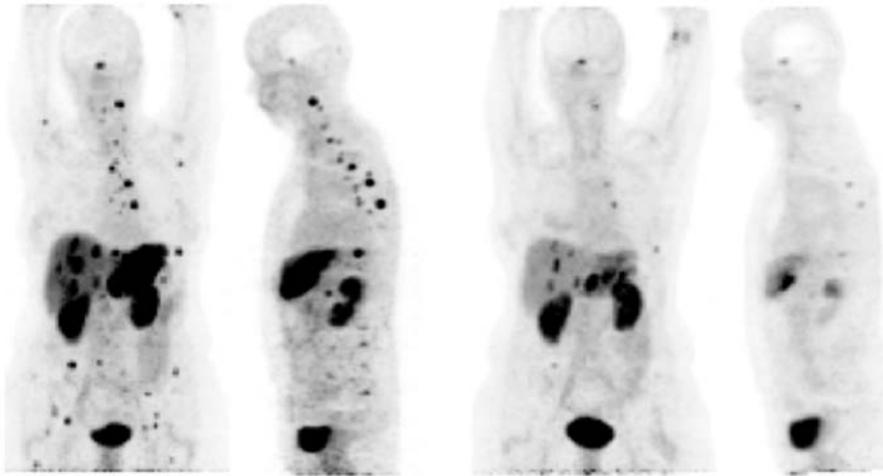
# With Large Infrastructure



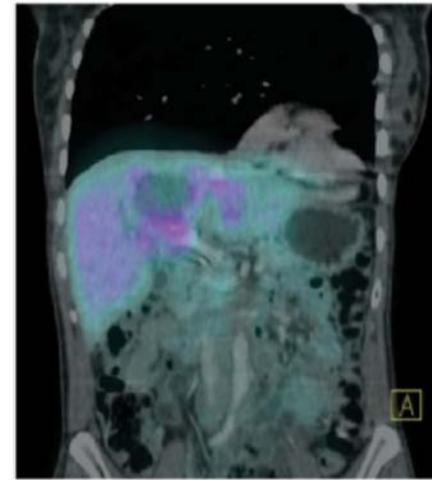




# Curative Appeal in People



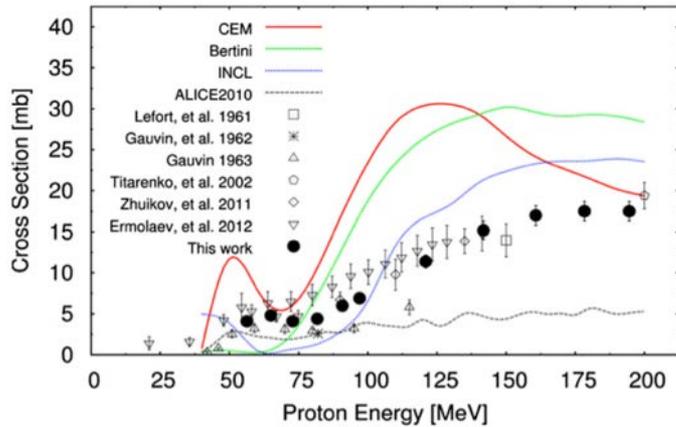
Case I: Shrinkage of liver lesions and bone metastases after i.a. therapy with 11 GBq Bi-213-DOTATOC



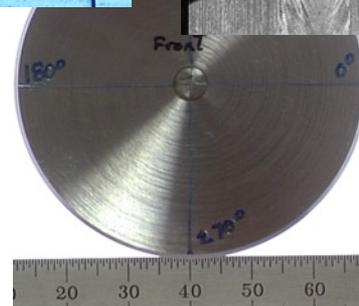
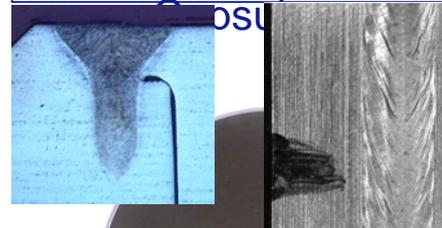
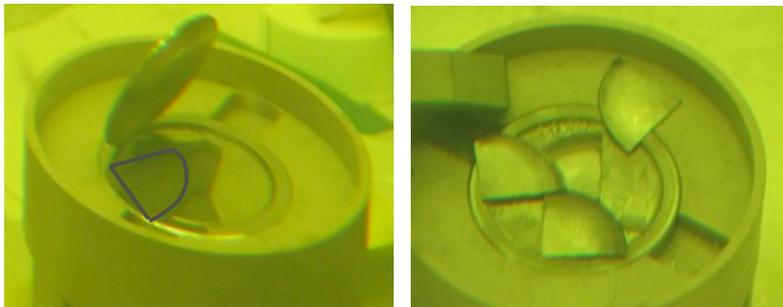
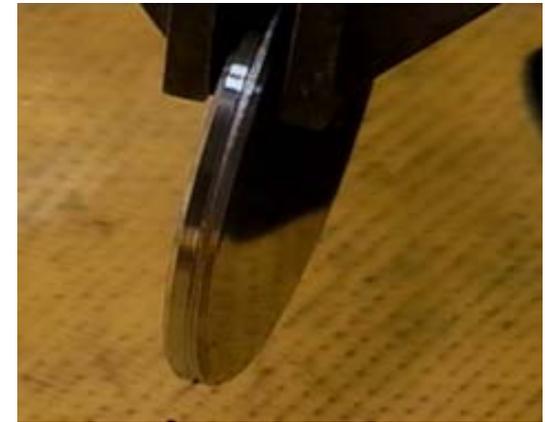
Case II: Response of multiple liver lesions after i.a. therapy with 14 GBq Bi-213-DOTATOC



# Th-232(p,x)Ac-225 for Alpha Radiotherapy

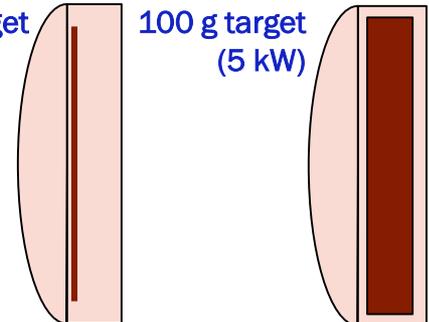


Electron Beam  
Welded Inconel



10 g target  
(0.5 kW)

100 g target  
(5 kW)



- Up to 7 day Irradiations at 230  $\mu$ A
- Ci-scale yields of  $^{225}\text{Ac}$
- 20x the Current Global Annual Supply



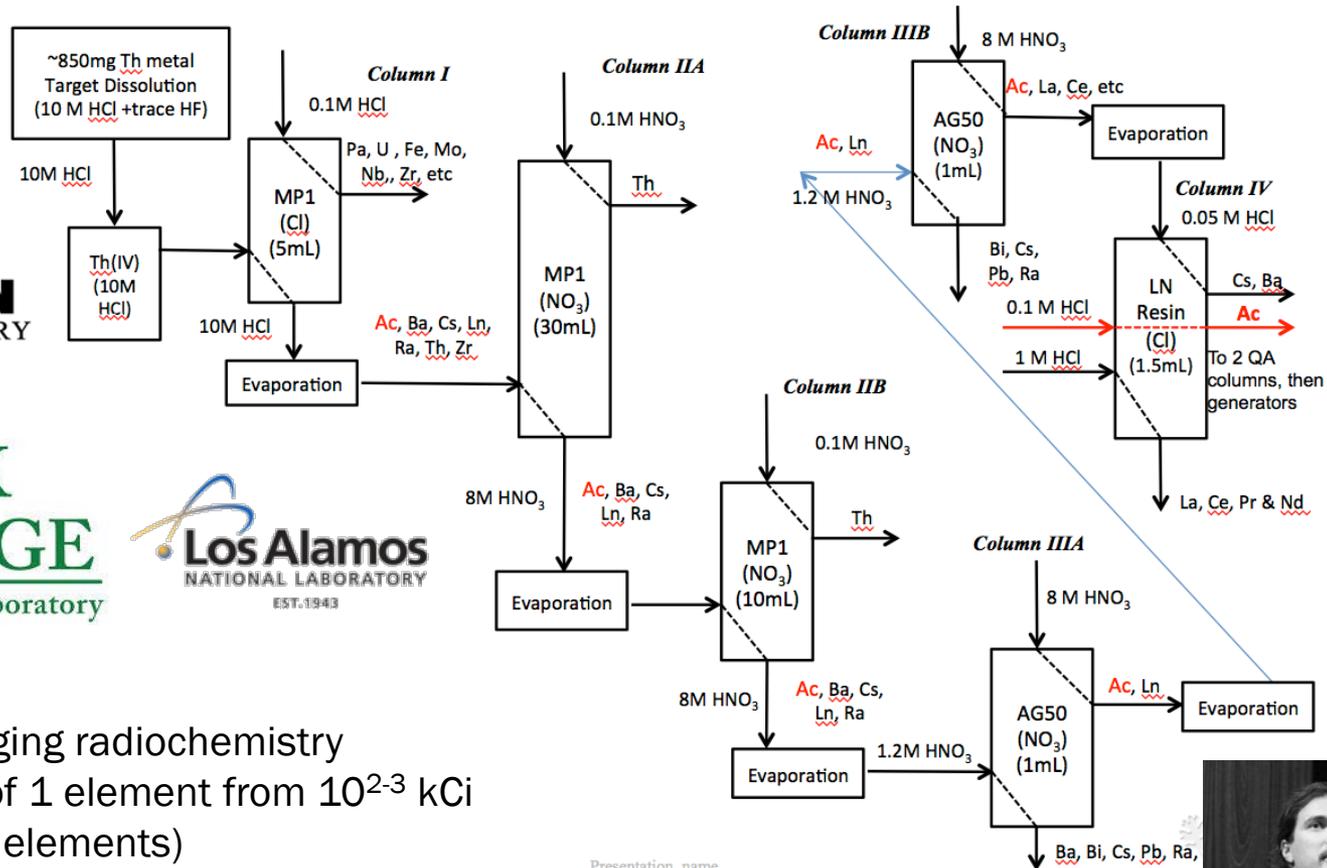
# Isolating $^{225}\text{Ac}$ from Irradiated Thorium

**BROOKHAVEN**  
NATIONAL LABORATORY

**OAK  
RIDGE**  
National Laboratory

**Los Alamos**  
NATIONAL LABORATORY  
EST. 1943

- Very Challenging radiochemistry (separation of 1 element from  $10^{2-3}$  kCi of 70+ other elements)
- Light lanthanides were a significant challenge (require 2 additional columns in the process)



Presentation\_name

Radchenko et al., *J Chrom A*, 2014

Dr. Valery Radchenko





# The Appealing Landscape

- $^{225}\text{Ac}$  ( $^{213}\text{Bi}$ )
  - $^{232}\text{Th}(p,x)^{225}\text{Ac}$
  - $^{226}\text{Ra}(p,2n)^{225}\text{Ac}$
  - $^{226}\text{Ra}(n,\gamma)(n,\gamma)(n,\gamma)^{229}\text{Th} \rightarrow ^{225}\text{Ra} \rightarrow ^{225}\text{Ac}$
  - $^{226}\text{Ra}(\gamma,p)$  or  $(\gamma,2n)^{225}\text{Ra} \rightarrow ^{225}\text{Ac}$
- $^{212}\text{Bi}$ 
  - Reactor production of  $^{228}\text{Th}$ , multiple routes
- $^{227}\text{Th}$  ( $^{223}\text{Ra}$ )
  - Reactor production of  $^{227}\text{Ac}$ , multiple routes from  $^{226}\text{Ra}$
  - The sole FDA-approved alpha-emitting radiopharmaceutical =  $^{223}\text{RaCl}_2$
- $^{230}\text{Pa}/^{230}\text{U}$  ( $^{226}\text{Th}$ )
  - $^{232}\text{Th}(p,3n)^{230}\text{Pa}$
- $^{149}\text{Tb}$ 
  - Multiple high energy charged particle spallation routes, ALL followed by online mass separation.
- $^{211}\text{At}$ 
  - $^{209}\text{Bi}(\alpha,2n)^{211}\text{At}$
  - $^{209}\text{Bi}(^7\text{Li},5n)$  or  $^{209}\text{Bi}(^6\text{Li},4n)^{211}\text{Rn} \rightarrow ^{211}\text{At}$



# Untenable (?) Cost

- National Radionuclide Providers operate under full-cost recovery models.
- Historically, industry takes over when a radionuclide becomes commercially viable.
- Commercial viability is harder to achieve when industry has to duplicate infrastructure at National Scales

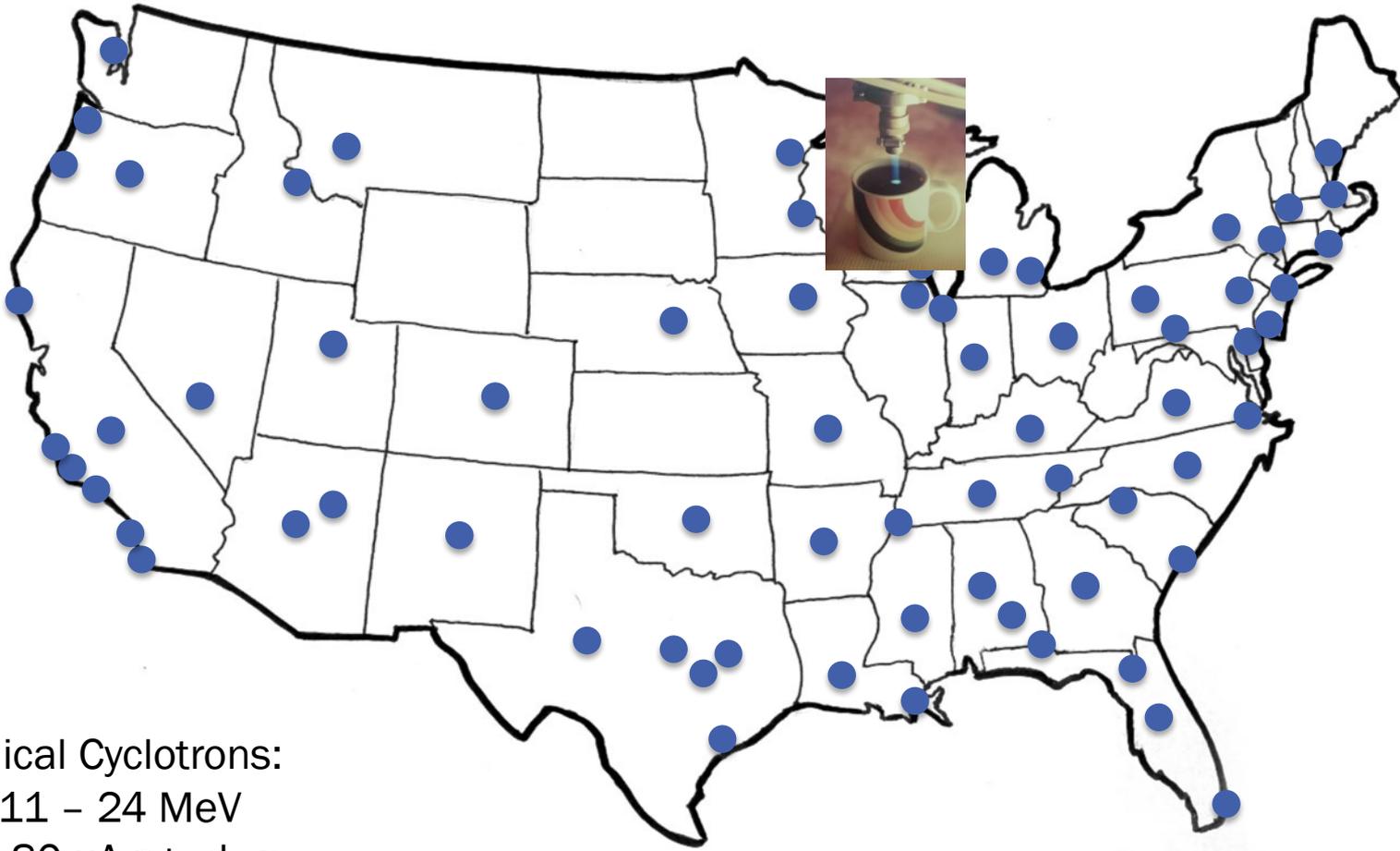


# Gedankenexperiment

- Current Annual Supply of  $^{225}\text{Ac}$  ~ 1 Ci  
(140 mCi every 6-8 weeks from ORNL  $^{229}\text{Th}$  cow)
- Supply Increase from IPF + BLIP at Full Capacity ~ x50  
... or about 50 Ci
- 1 Treatment of  $^{225}\text{Ac}$ -derived  $^{213}\text{Bi}$  (the clinically-demonstrated agents) ~ 80 mCi →  $10^2$  patients/yr  
(3 rounds of therapy each)
- 3 Treatments of  $^{225}\text{Ac}$ -labeled targeting vector per patient at ~ 1 mCi each →  $10^4$  patients/yr
- 14M Cancer Patients exist in the US at any one time.
  - So.... What to do...



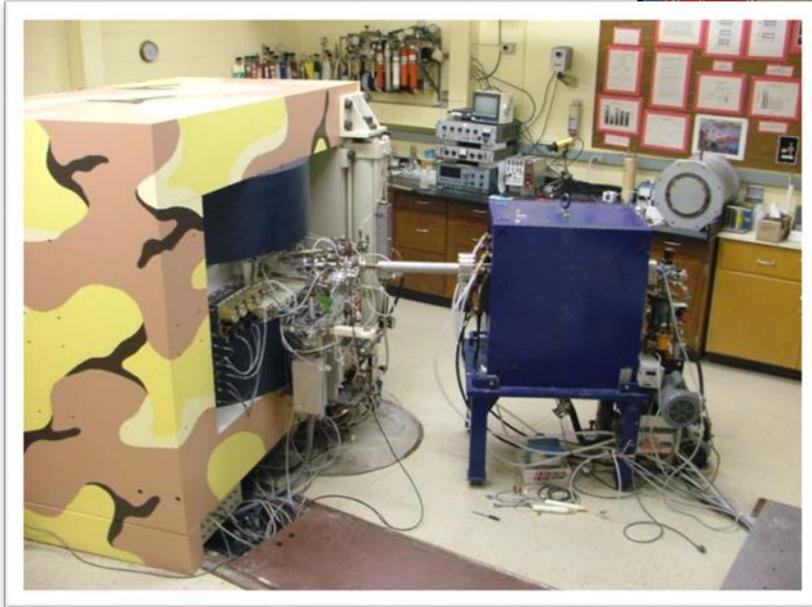
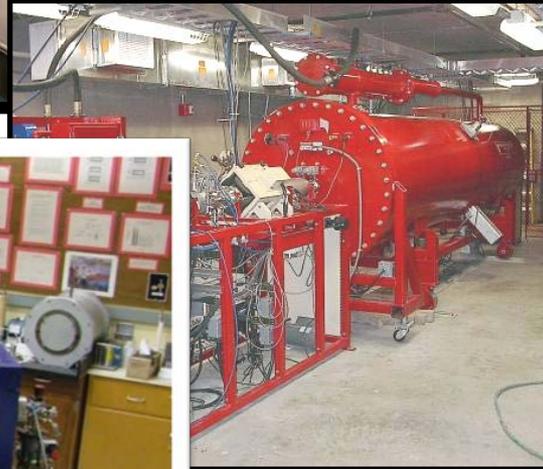
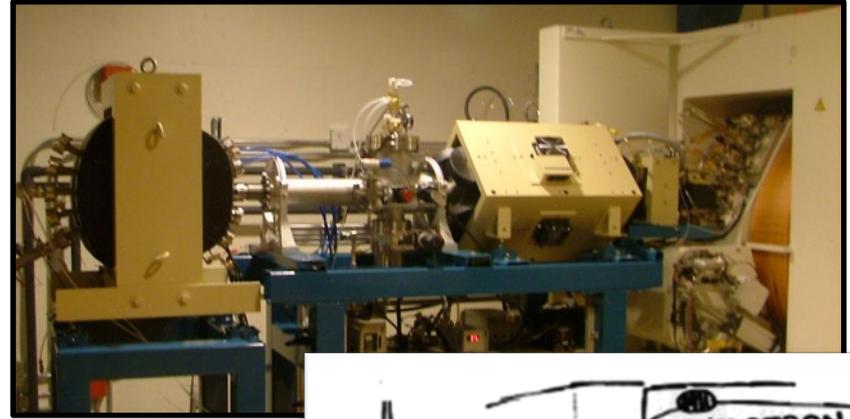
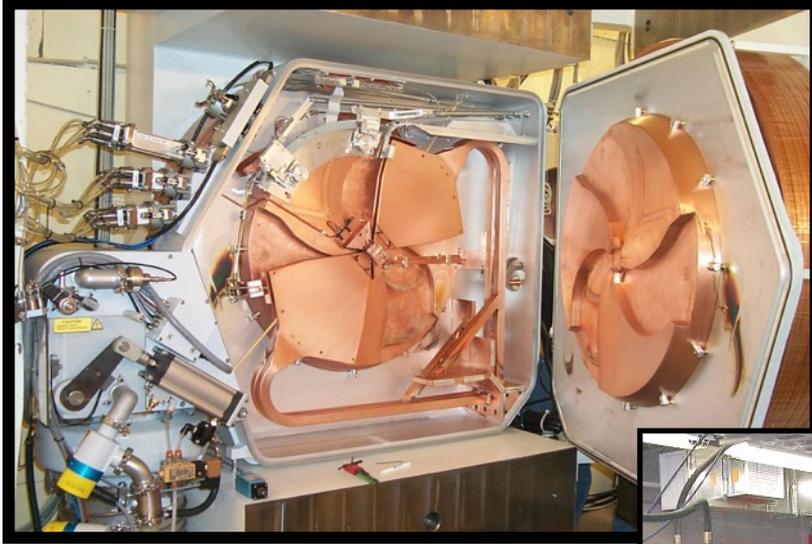
# The Distributed Small-Cyclotron Network of Radionuclide-Producing Facilities



Medical Cyclotrons:  
~ 11 - 24 MeV  
10 - 80  $\mu$ A p+, d,  $\alpha$

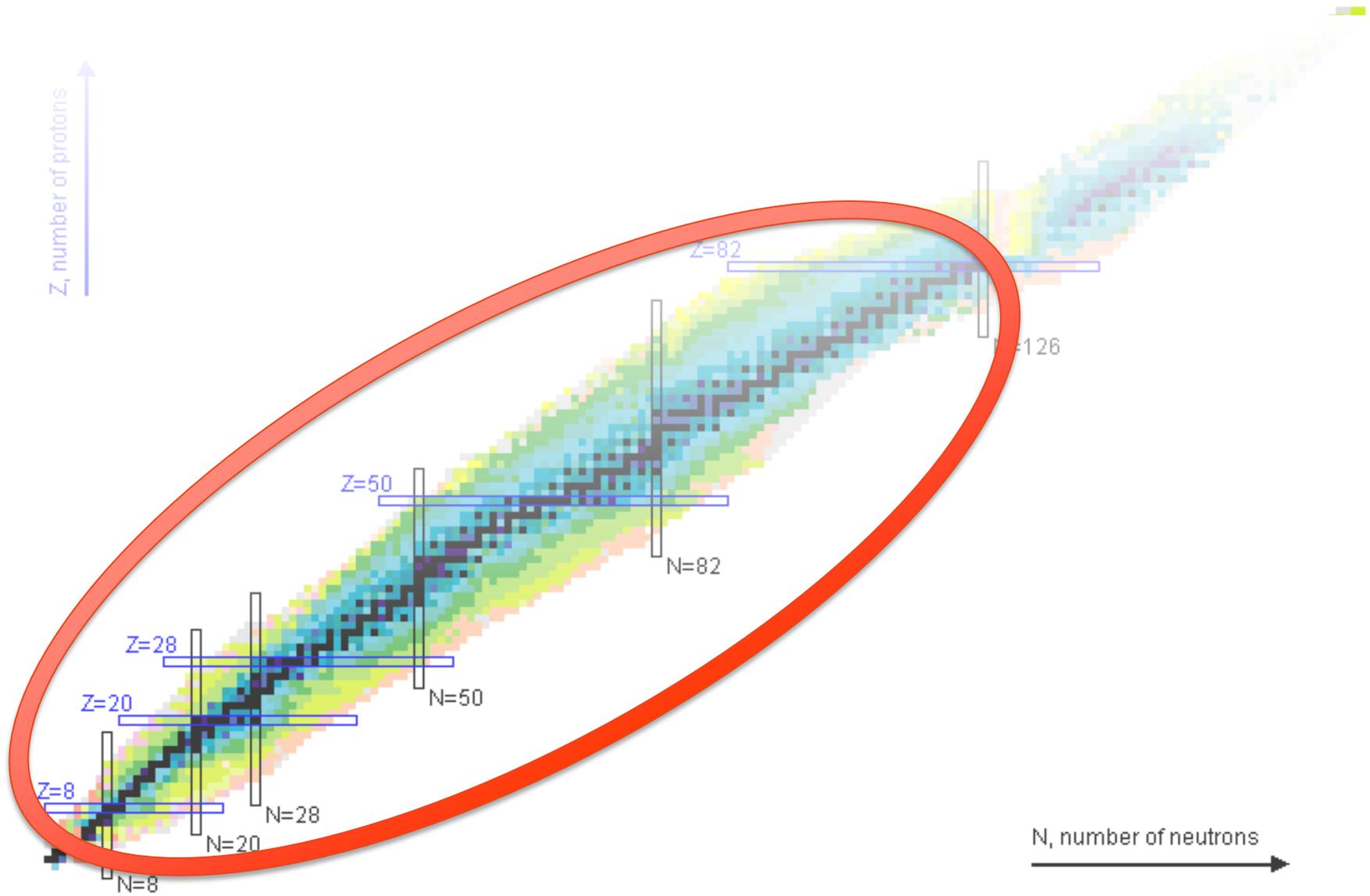


# Shoot





# With Small Cyclotrons





# The Menu du Jour

<u>Nuclide</u>	<u>t<sub>1/2</sub></u>	<u>Reaction</u>	<u>%</u>	<u>Yield (EoSb)</u>	<u>SA</u>	<u>Synthon</u>	<u>Status</u>
● <sup>34m</sup> Cl	32 m	<sup>36</sup> Ar(d,α)	0.3	4.6 mCi/μA	-	Cl <sup>-</sup> , ClF	animal imaging
● <sup>44</sup> Sc	3.9 h	<sup>44</sup> Ca(p,n)	2	5.8	1	Sc <sup>3+</sup>	animal imaging
● <sup>45</sup> Ti	3.1 h	<sup>45</sup> Sc(p,n)	100	47	1	TiCl <sub>4</sub>	animal imaging
● <sup>51</sup> Mn	46 m.	<sup>54</sup> Fe(p, α)	5.8	26	1	Mn <sup>2+</sup>	animal imaging
● <sup>52g</sup> Mn	5.6 d	<sup>52</sup> Cr(p,x)	82	0.3	1	Mn <sup>2+</sup>	animal imaging
● <sup>61</sup> Cu	3.4 h	<sup>60</sup> Ni(d,n)	26	20	0.1	ATSM	patients
● <sup>64</sup> Cu	12.7 h	<sup>64</sup> Ni(p,n)	0.9	170	25	Cu <sup>2+</sup>	animals, distribution
● <sup>66</sup> Ga	9.6 h	<sup>66</sup> Zn(p,n)	28	31	20	Ga-NOTA	animal imaging
● <sup>68</sup> Ga	68 m	<sup>68</sup> Zn(p,n)	19	35	20	“	animal imaging
● <sup>72</sup> As	26 h	<sup>72</sup> Ge(p,n)	27	102	-	As <sup>3+</sup>	chem separation
● <sup>86</sup> Y	15 h	<sup>86</sup> Sr(p,n)	10	26	1.5	Y-DOTA	animal imaging
● <sup>89</sup> Zr	78 h	<sup>nat</sup> Y(p,n)	100	100	20	Zr-DFO	animals, distribution
● <sup>95m</sup> Tc	65 d	<sup>95</sup> Mo(p,n)	16	21	-	Tc-in-Mo	chemistry

inception



acceptance



In-house

few users

distribution

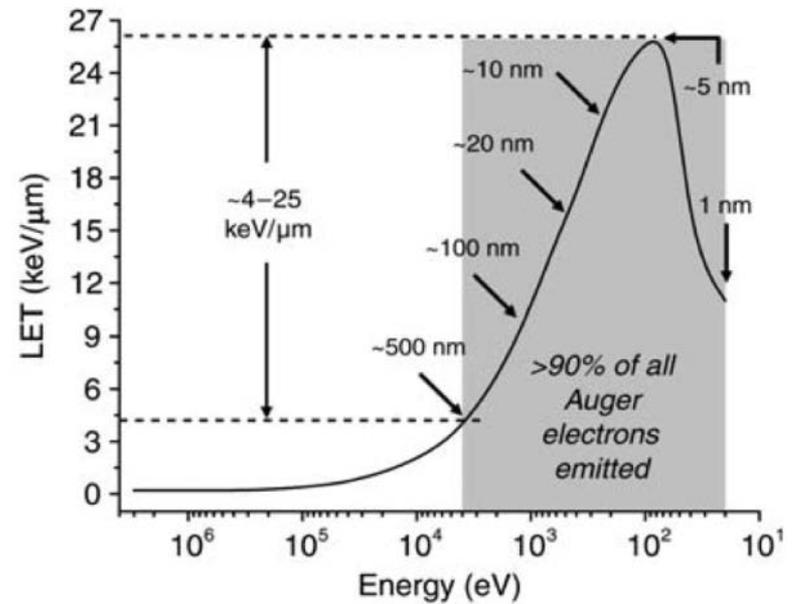
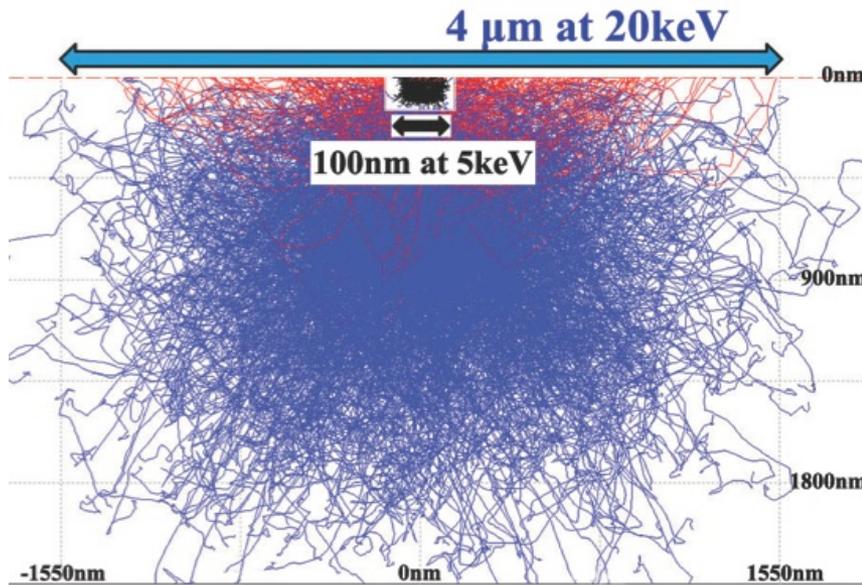


# Interesting Auger/Conversion Electron Emitters

- $^{111}\text{In}$ ,  $^{114\text{m}}\text{In}$
- $^{125}\text{I}$
- $^{94}\text{Tc}$ ,  $^{99\text{m}}\text{Tc}$
- $^{117\text{m}}\text{Sn}$
- $^{193\text{m}}\text{Pt}$ ,  $^{195\text{m}}\text{Pt}$
- $^{119}\text{Sb}$
- $^{58\text{m}}\text{Co}$
- $^{71}\text{Ge}$
- $^{77}\text{Br}$ ,  $^{80\text{m}}\text{Br}$
- $^{67}\text{Ga}$
- $^{103}\text{Ru}$
- $^{140}\text{Nd}/^{140}\text{Pr}$
- $^{161}\text{Tb}$
- $^{165}\text{Er}$
- $^{55}\text{Fe}$ ,  $^{57}\text{Fe}$ ,  $^{59}\text{Fe}$
- $^{197}\text{Hg}$
- $^{201}\text{Tl}$
- $^{158}\text{Gd}$  (from  $n, \gamma$ ),  $^{159}\text{Gd}$
- $^{131}\text{Cs}$
- $^{51}\text{Cr}$
- $^{103}\text{Pd}$
- $^{167}\text{Tm}$
- $^{178}\text{Ta}$



# High-LET Augers?



A.I. Kassis, Rad. Prot. Dosimetry 143 (2011) 241.

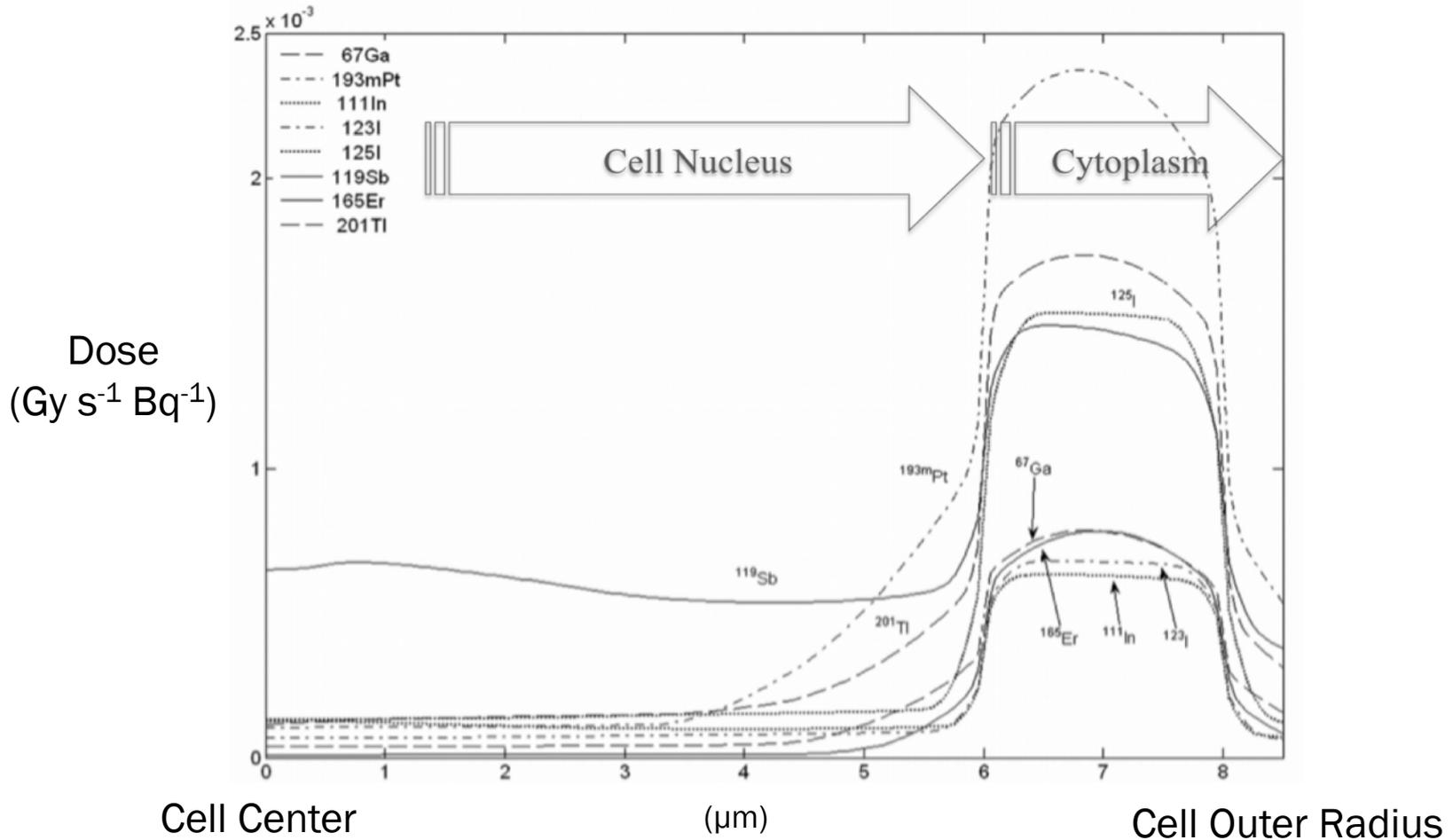


## **ICRP publication 92: Relative Biological Effectiveness (RBE), Quality Factor (Q), and Radiation Weighting Factor ( $w_R$ )**

“....For **Auger** emitters bound to DNA, high RBE values have been reported and a  $w_R$  of 20 or more appears to be appropriate. For those **Auger** electron emitters that enter the cell but are not bound to DNA, RBE values between 1.5 and 8 have been found for different endpoints in cell studies (Kassis et al., 1987; Makrigiorgios et al., 1990). Even the less critical case of more uniformly distributed **Auger** emitters should, therefore, be included in future considerations on a convention for  $w_R$  values for **Auger** electron emitters.”



# Variable electron emission spectra → Variable cellular dosimetry





# Nuclear Formation Reaction Data

## Nuclear Data Needs and Capabilities for Applications

May 27-29, 2015

Lawrence Berkeley National Laboratory,  
Berkeley, CA USA

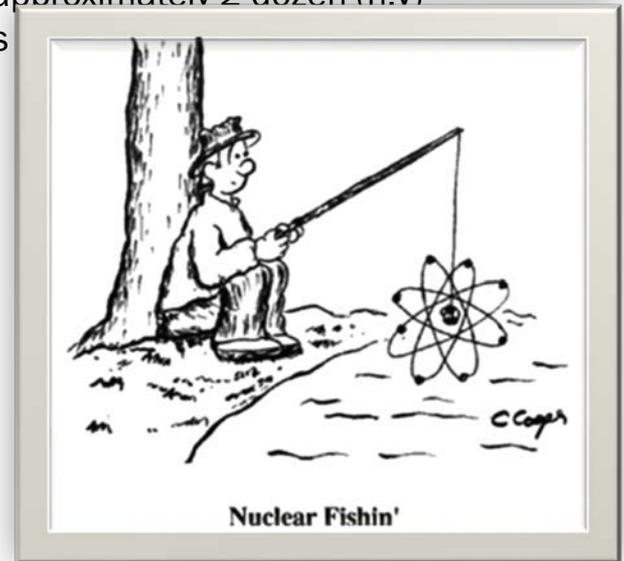


For medical radionuclides:

$^{191}\text{Ir}(n,\gamma)$ ,  $^{192}\text{Os}(d,n)^{192}\text{Ir}$ ,  $^{130}\text{Te}(n,\gamma)^{131}\text{Te} \rightarrow ^{131}\text{I}$ ,  
 $^{130}\text{Te}(d,p)^{131}\text{Te} \rightarrow ^{131}\text{I}$ ,  $^{130}\text{Te}(d,n)^{131}\text{I}$ ,  $^{187}\text{Re}(d,p)^{188}\text{Re}$ ,  
 $^{152}\text{Sm}(n,\gamma)^{153}\text{Sm}$ ,  $^{150}\text{Nd}(\alpha,n)^{153}\text{Sm}$ ,  $^{185}\text{Re}(n,g)^{186}\text{Re}$ ,  
 $^{186}\text{W}(p,n)^{186}\text{Re}$ ,  $^{89}\text{Y}(n,\gamma)^{90}\text{Y}$ , many reactions to  
produce  $^{125}\text{I}$ ,  $^{89}\text{Sr}(n,\gamma)^{90}\text{Sr}$ ,  $^{32}\text{S}(d,2p)^{32}\text{P}$ , multiple  
reactions esp. fast neutrons to produce  $^{99}\text{Mo}$ ,  
 $^{226}\text{Ra}(\gamma,n)^{225}\text{Fr} \rightarrow ^{225}\text{Ra} \rightarrow ^{225}\text{Ac}$ ,  $^{226}\text{Ra}(n,x)^{225}\text{Ac}$ ,  
 $^{226}\text{Ra}(n,x)^{227}\text{Ac}$ ,  $^{131}\text{Xe}(p,n)^{131}\text{Cs}$ ,  $^{154}\text{Sm}(n,x)^{155}\text{Eu}$   
(fast),  $^{130}\text{Te}(\alpha,np)^{132}\text{I}$ ,  $^{176}\text{Yb}(d,n)^{177}\text{Lu}$ ,  
 $^{53}\text{Cr}(d,n)^{54}\text{Mn}$ ,  $^{\text{nat}}\text{Fe}(p,x)^{52}\text{Mn}$ ,  $^{94}\text{Zr}(n,\gamma)^{95}\text{Zr} \rightarrow ^{95}\text{Nb}$ ,  
 $^{\text{nat}}\text{Br}(p,x)^{75}\text{Se}$ ,  $^{\text{nat}}\text{I}(p,x)^{127}\text{Xe}$ ,  $^{\text{nat}}\text{Tm}(p,x)^{169}\text{Yb}$ ,  
 $^{91}\text{Zr}(n,p)^{91}\text{Y}$ , approximately 2 dozen (n.v)  
radionuclides

### Ultra Low Energy Electrons (ULEE, 0-20 eV)

- not contained in the International Commission on Radiological Protection (ICRP) nor in the Medical Internal Radiation Dose (MIRD) data bases
- Substantial contribution to the overall absorbed dose and to molecular damage
- Strong correlation between stopping cross section and biological damage (double strand Breaks)





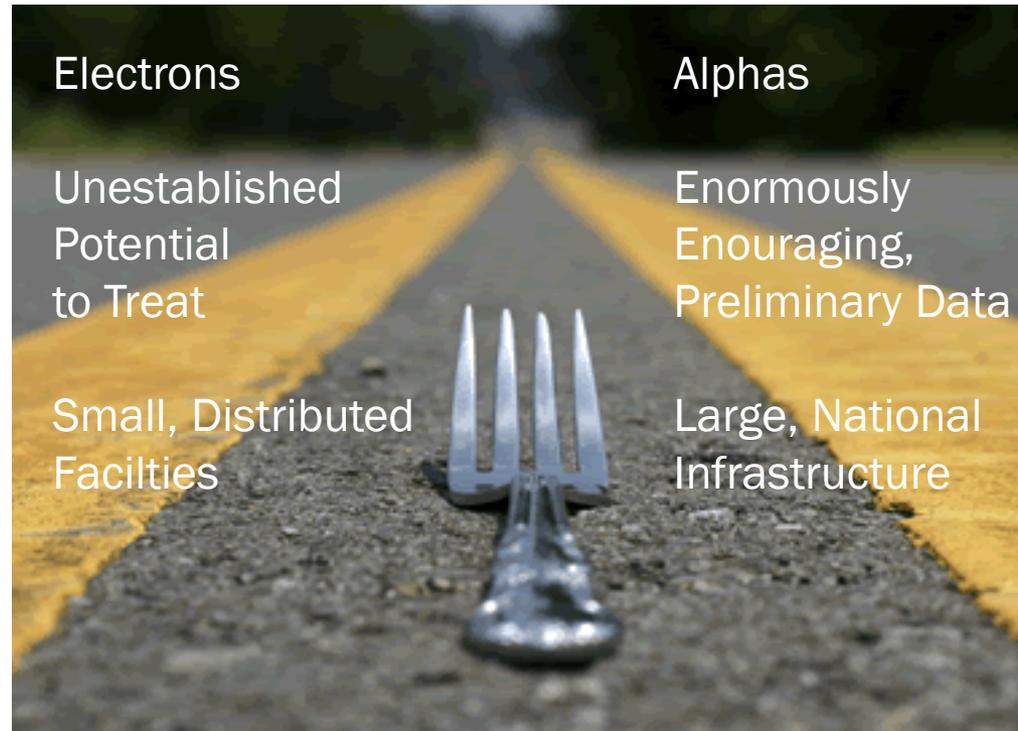
# Gaps in Nuclear Structure Data, Weakness in Current Calculation Models

**Table 1.** Calculated Auger electron yield per nuclear decay for selected medical radioisotopes.

	RADAR <sup>a</sup>	DDEP <sup>a</sup>	Eckerman & Endo <sup>a</sup>	Howell <sup>b</sup>	Stepanek <sup>b</sup>	Pomplun <sup>b</sup>	Nikjoo <sup>b</sup>
	[13, 14]	[15]	[16]	[17]	[18]	[19, 20]	[6]
<sup>99m</sup> Tc (6.007 h)	0.122	0.13	4.363	4.0		2.5	
<sup>111</sup> In (2.805 d)	1.136	1.16	7.215	14.7	6.05		
<sup>123</sup> I (13.22 h)	1.064	1.08	13.71	14.9		6.4	
<sup>125</sup> I (59.4 d)	1.77	1.78	23.0	24.9	15.3	12.2	20.2
<sup>131</sup> Cs (9.689 d)	0.4745		10.7				
<sup>201</sup> Tl (3.04 d)	0.773	0.614	20.9	36.9			



# Summary





# Acknowledgements

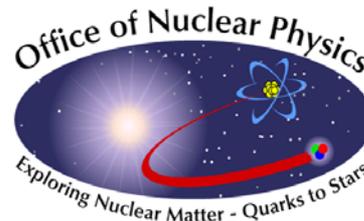


**WISCONSIN**  
UNIVERSITY OF WISCONSIN-MADISON

Jerry Nickles  
Todd Barnhart  
Paul Ellison  
Steven Graves  
Hector Valdovinos



Eva Birnbaum  
Meiring Nortier  
Kevin John  
Wayne Taylor  
Kevin Jackman  
Stepan Mashnik  
Mark Brugh  
Justin Wilson



Valery Radchenko  
Michelle Mosby  
Lauren Marus  
Joel Maassen  
David Reass  
Mike Connors  
Don Dry  
Stosh Kozimor

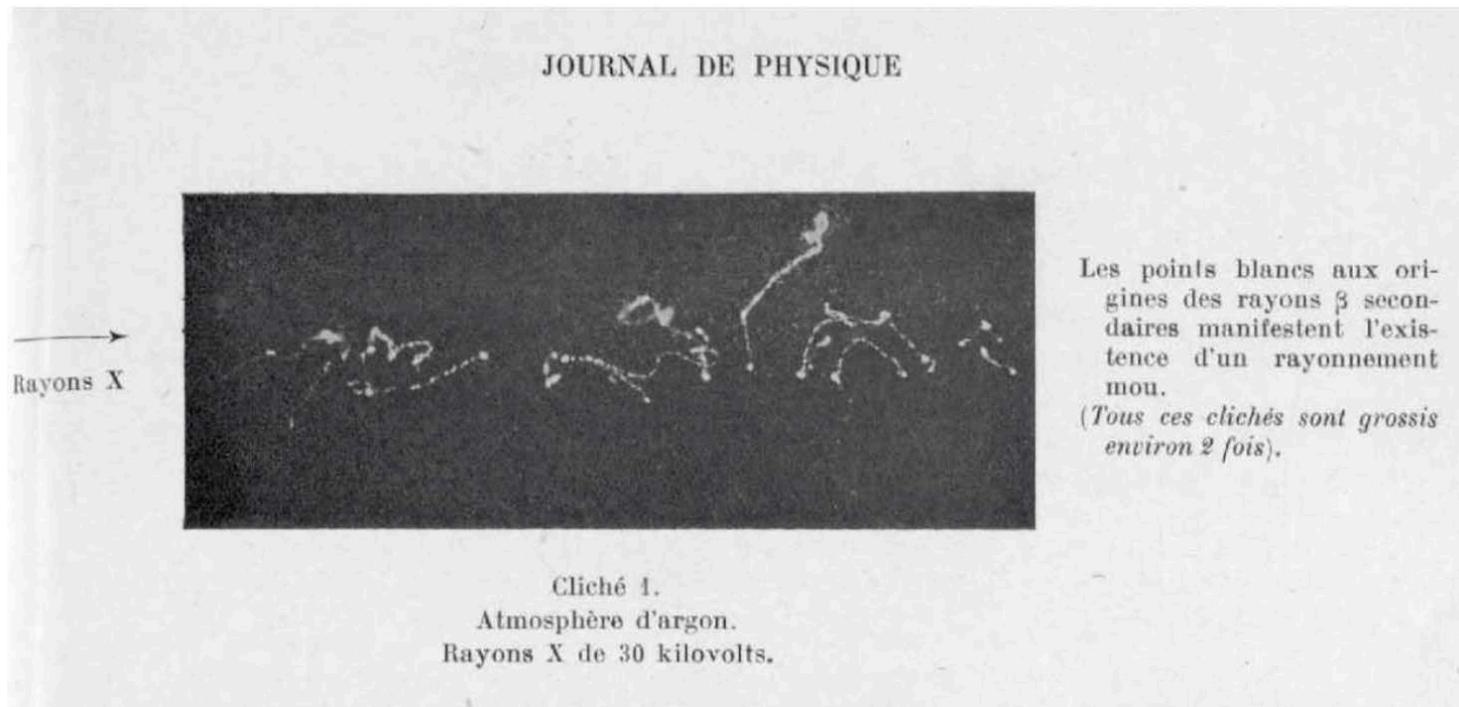


Dennis Phillips  
Mark Garland  
Joel Grimm  
Mitch Ferren  
Cassie Dukes

Cleo Naranjo  
Michael Gallegos  
Dave Thorn  
Michael Fassbender  
Maryline Ferrier  
Justin Wilson  
Benjamin Stein  
Veronika Mocko... and many others



# Thank you for your kind attention.



P. Auger

Journal de Physique et le Radium, 6 (1925) 205.