

# Numerical and Experimental Feasibility Study of HDR $^{192}\text{Ir}$ Brachytherapy Water Calorimetry

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# $^{192}\text{Ir}$ Brachytherapy Dosimetry

$$D_{\text{water}}(\bar{r})$$

TG-43

$$S_{K,\text{air}}$$

Calibrated  
well-type chamber

ADCL\*

PSDL<sup>+</sup>

Interpolation of air kerma calibration of a thimble type chamber based on its KV and  $^{137}\text{Cs}/^{60}\text{Co}$  calibration factors.

Cavity ionization chamber with correction for non-validity of Spencer Attix.

\* Accredited Dosimetry Calibration Laboratories

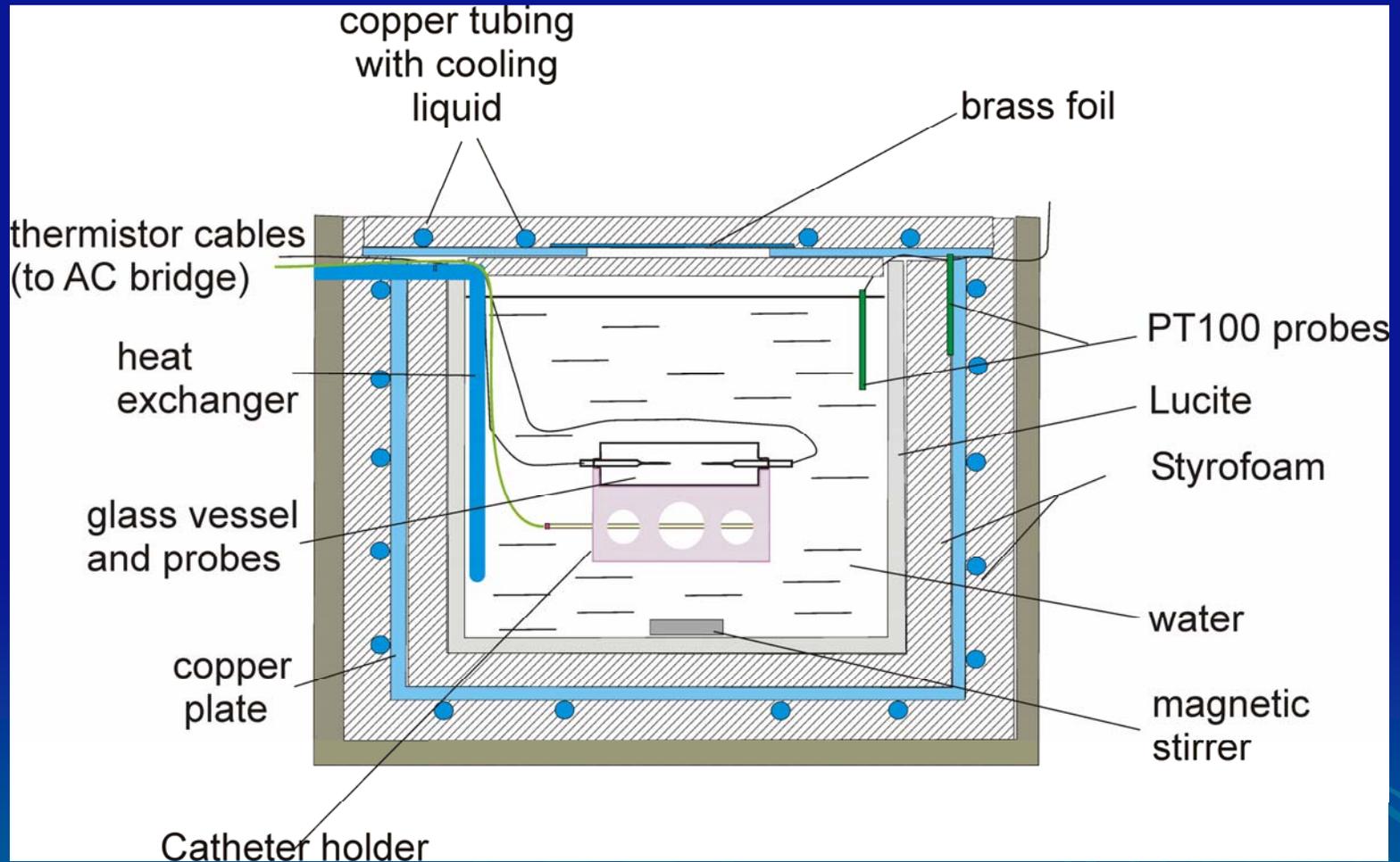
<sup>+</sup>Primary Standard Dosimetry Laboratories

# Brachytherapy Water Calorimetry

➤ **Difficulties:**  $D_w(\bar{r}) = c_w \cdot \Delta T(\bar{r}) \cdot \prod k_i$

- Sub-mK level temperature rise to be measured with sub-percent precision.
- Correction factors due to:
  - Heat transport (non-water materials & radiation dose gradient)
  - Heat defect (differences in energy absorbed and measured due to chemical reactions in water)
- Sharp dose gradient of the source
- Inherent self-heating of the source
- Accurate positioning of the source

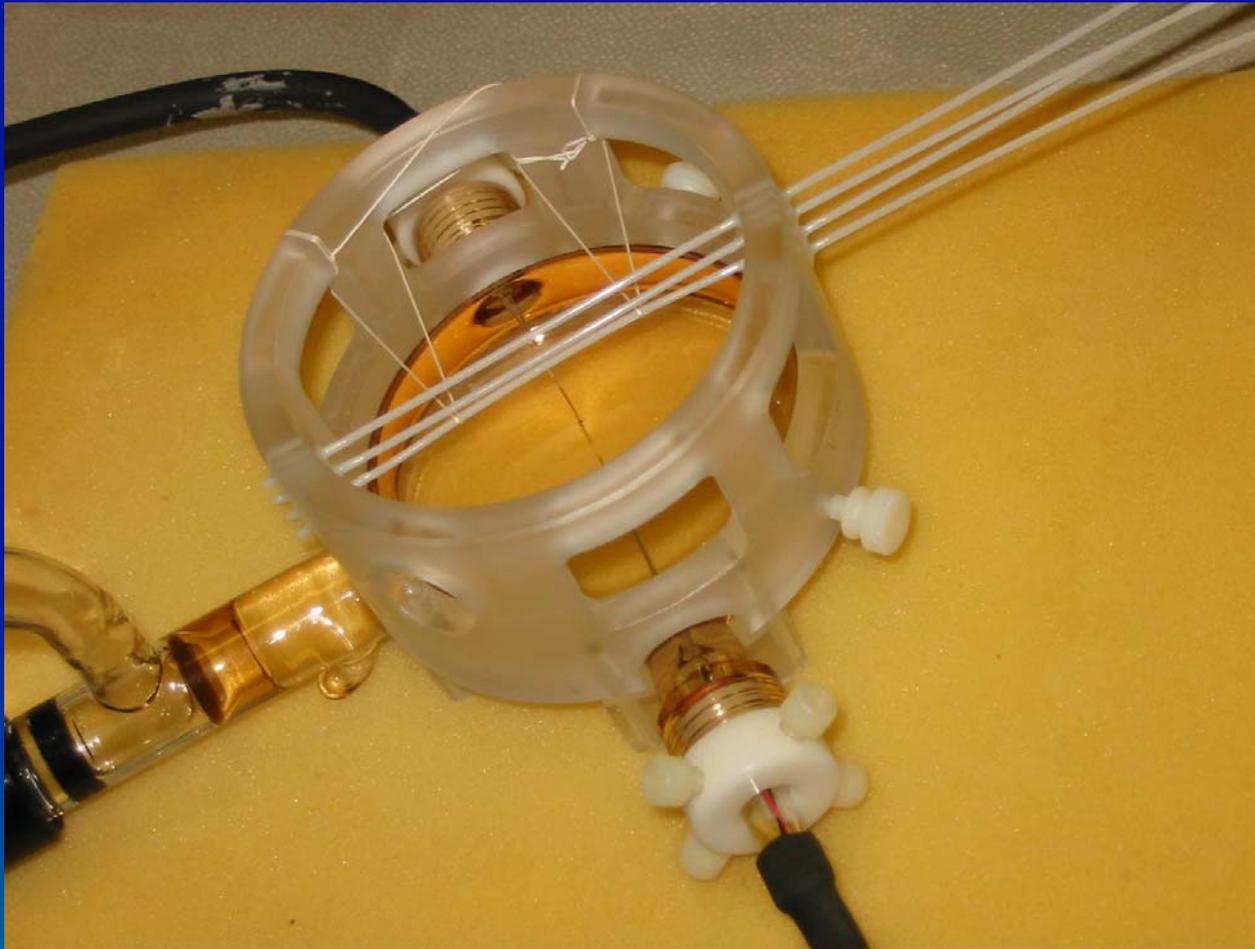
# Water Calorimetry



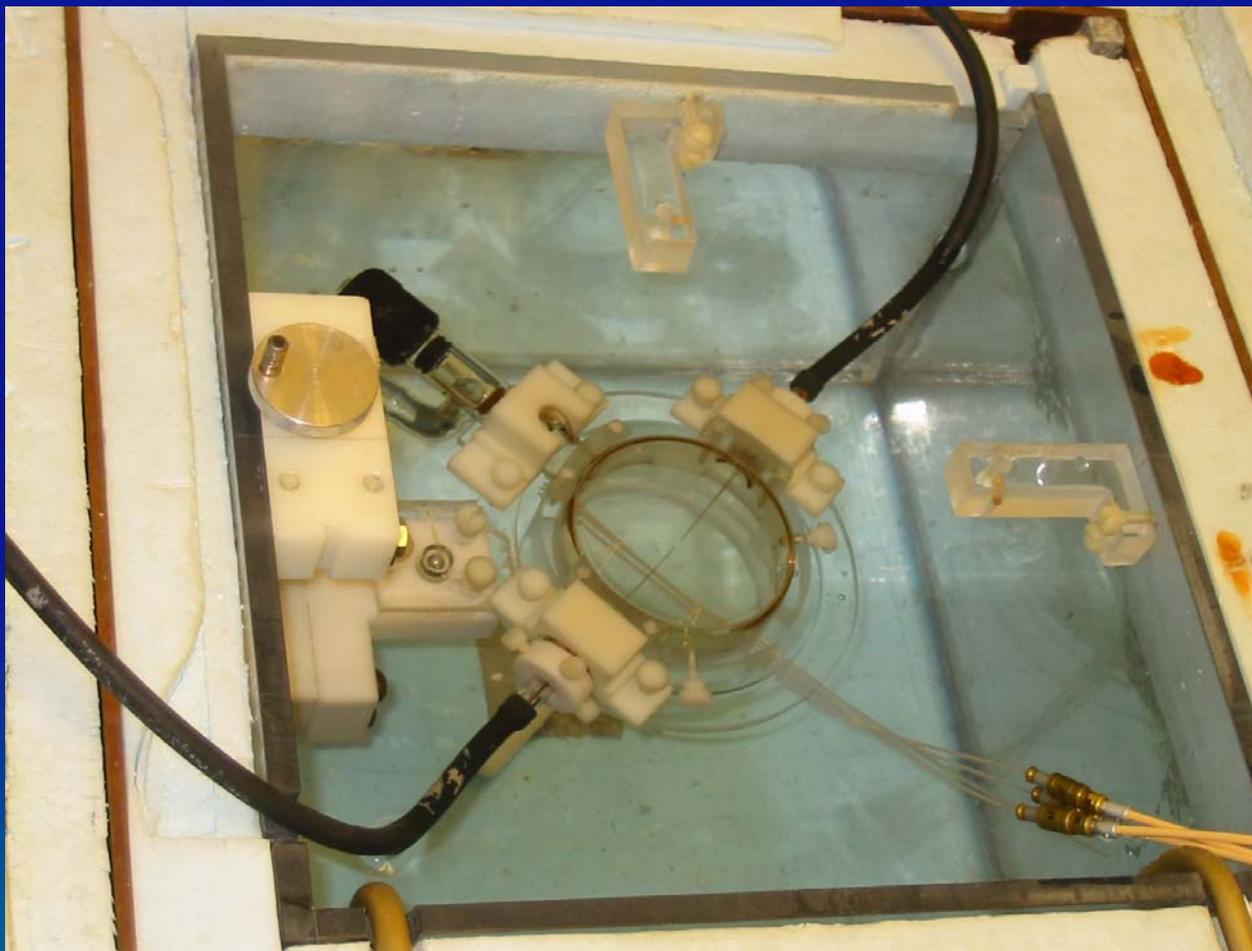
# Experimental Setup



# Experimental Setup

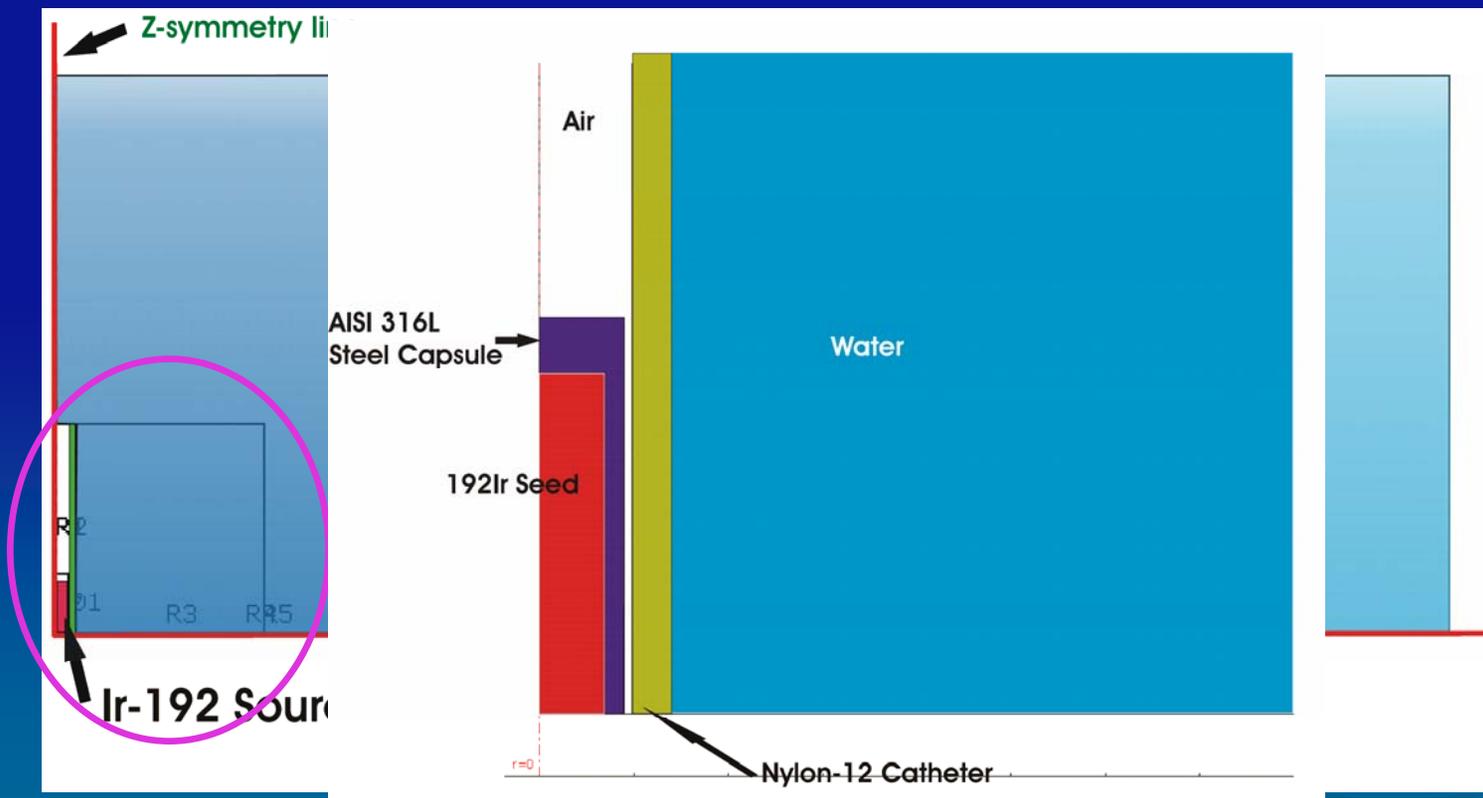


# Experimental Setup

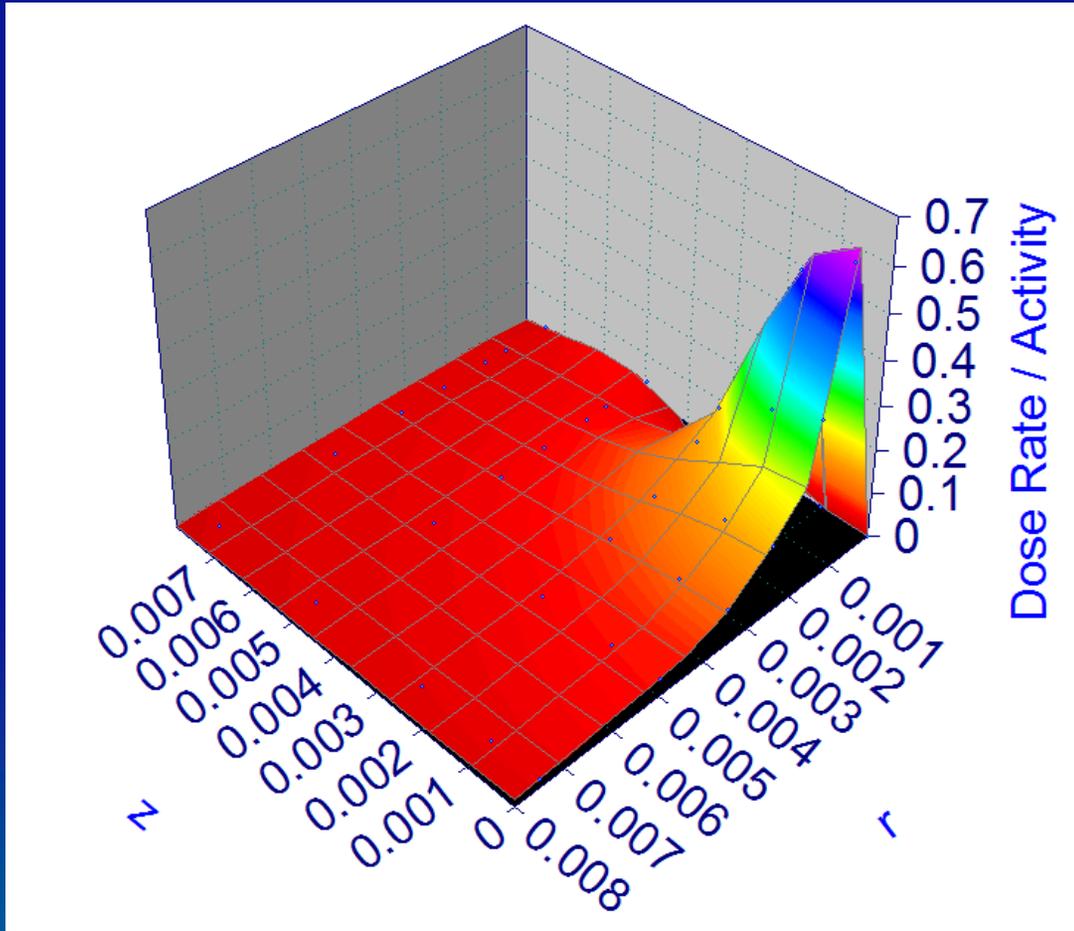


# Heat Transport Calculations

- Comsol Multiphysics™ Solves the *heat transport* equation (the partial differential equation) using the *finite element method*.



# Dose Distribution

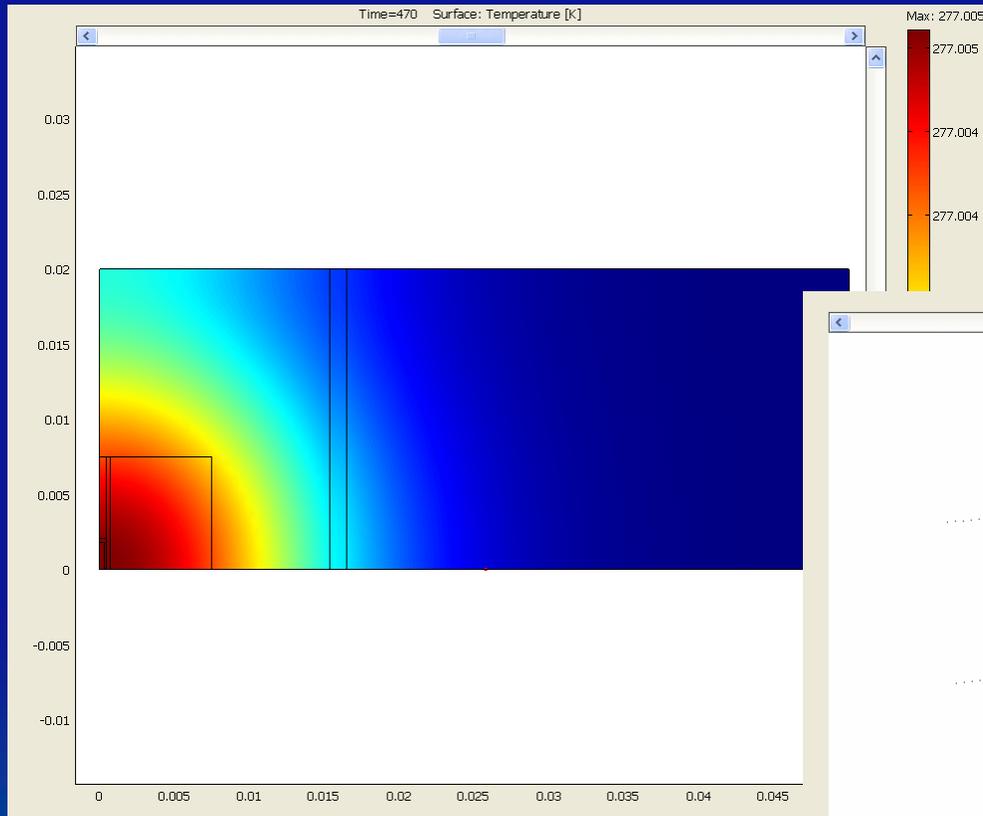


The fractional source self-dissipation due to self-attenuation of  $^{192}\text{Ir}$  photons and electrons in the source was calculated using EGSnrcMP code.

$D_{core}$	$1.79 \times 10^{-7}$ cGy/disintegration
$D_{capsule}$	$1.50 \times 10^{-8}$ cGy/disintegration
$S_{K,air}$	$3.80 \times 10^{-11}$ cGy.cm <sup>2</sup> /disintegration

G. M. Daskalov, E. Loffler, and J. F. Williamson, "Monte Carlo-aided dosimetry of a new high dose-rate brachytherapy source," Med. Phys. 25, 2200 (1998).

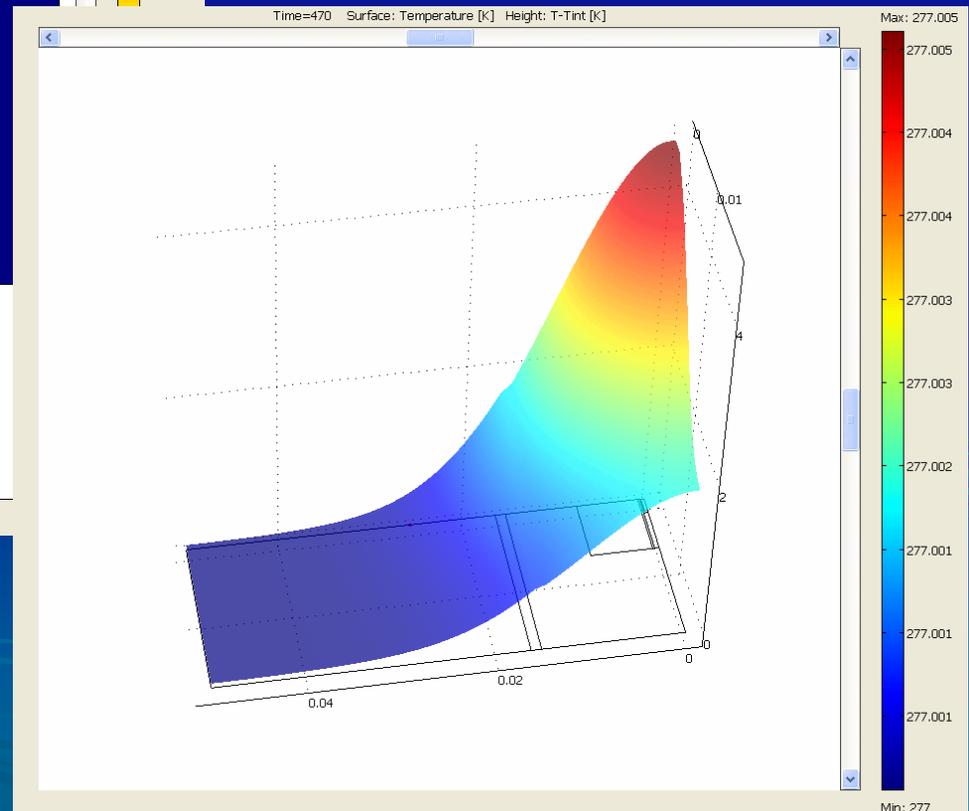
# Heat Transport Results



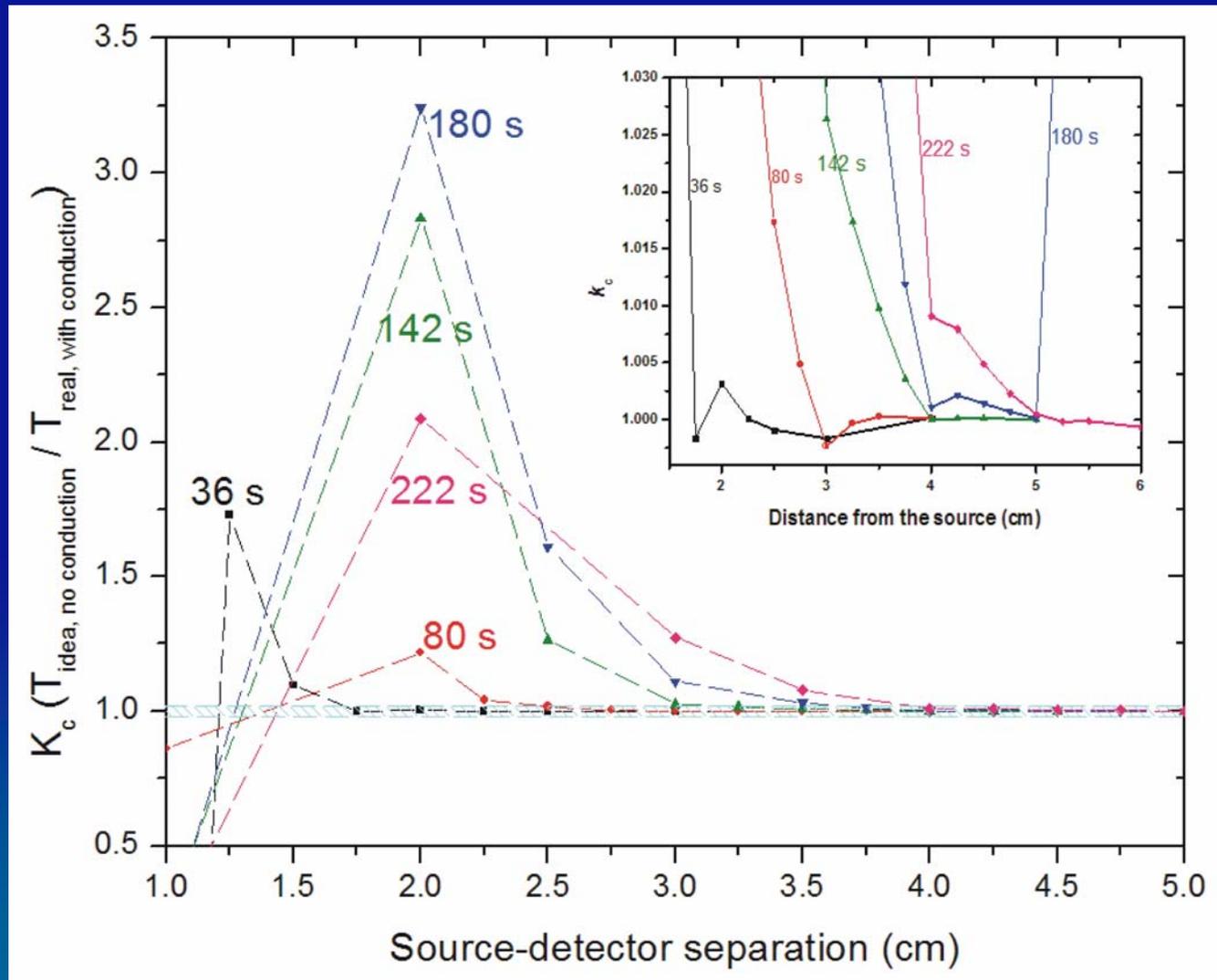
Source Activity: 5.049 Ci

Irradiation time: 70 s

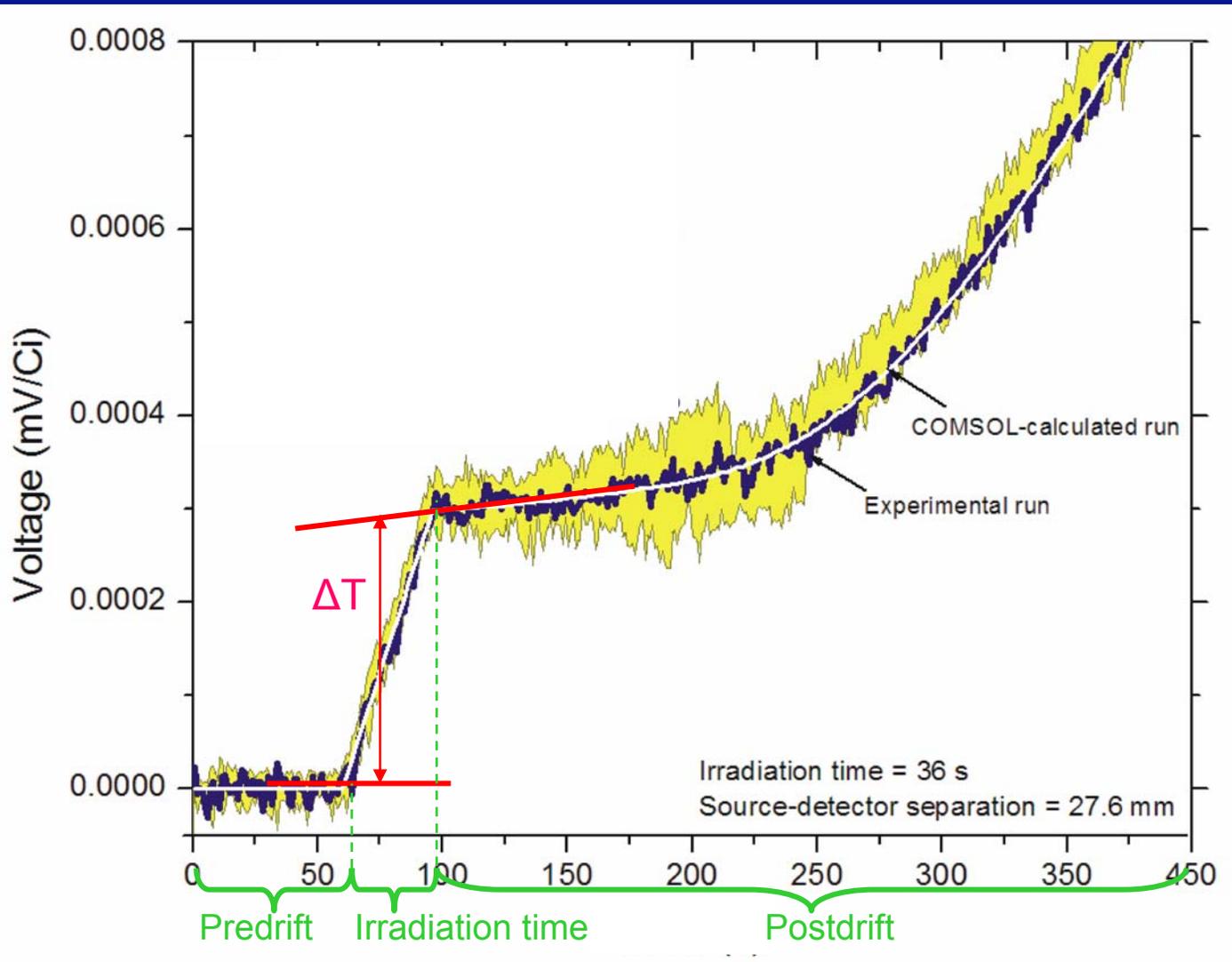
Post-drift: 400 s



# Conduction Correction Factor



# Measurement vs. Calculation



# Summary of Results

Nominal Source activity [Ci]	Source-detector separation [mm]	Irradiation time [s]	Number of calorimetric runs performed	Average dose rate [mGy/(s.Ci)]	TG-43 calculated dose rate [mGy/(s.Ci)]	% diff. exp. & TG-43
9.30	27.6±0.3	36	8	1.79±0.03	1.68	6.5
	26.4±0.4	50	7	1.82±0.03	1.83	0.3
5.05	26.8±0.5	80	3	1.84±0.09	1.83	0.6
	24.7±0.3	75	3	2.02±0.07	2.13	5.0
<b>AVERAGE</b>	<b>25</b>		<b>21</b>	<b>2.05±0.03</b>	<b>2.06</b>	<b>0.5</b>

# Conclusion

- HDR  $^{192}\text{Ir}$  brachytherapy water calorimetry is feasible.
- Absolute dose measurement with an uncertainty much better than 5% is achievable.
- Optimal point of measurement is between 2.5 to 6 cm from the source in the radial direction (on the perpendicular bisector) while ensuring that a minimum dose of 1 Gy is delivered.

# Acknowledgements

- Dr. K. Stewart
- Dr. E. Podgorsak
- R. Van Gils
- J. Larkin, B. Siva
- E. Poon

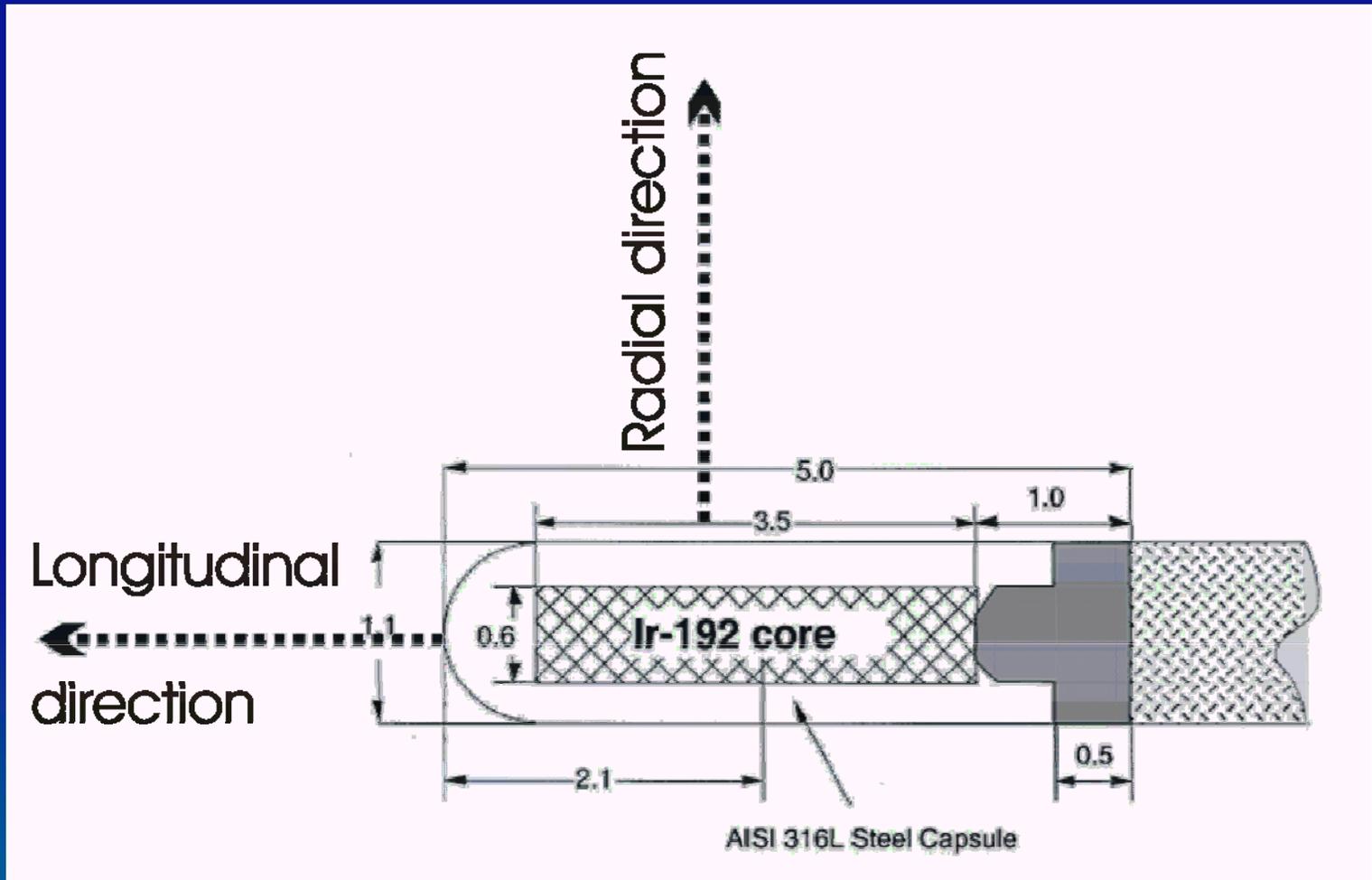


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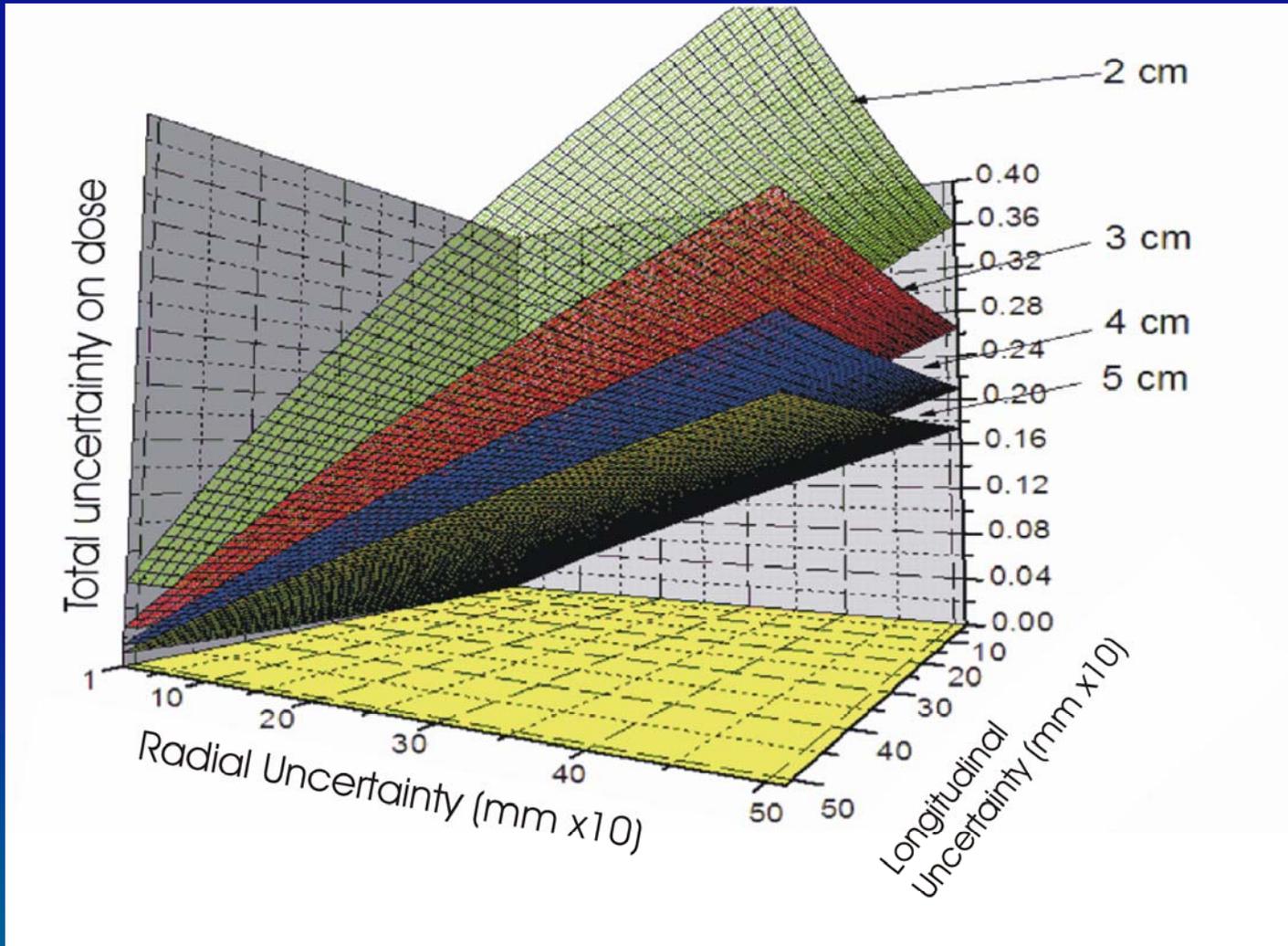


# Nucleotron microSelectron-HDR $^{192}\text{Ir}$

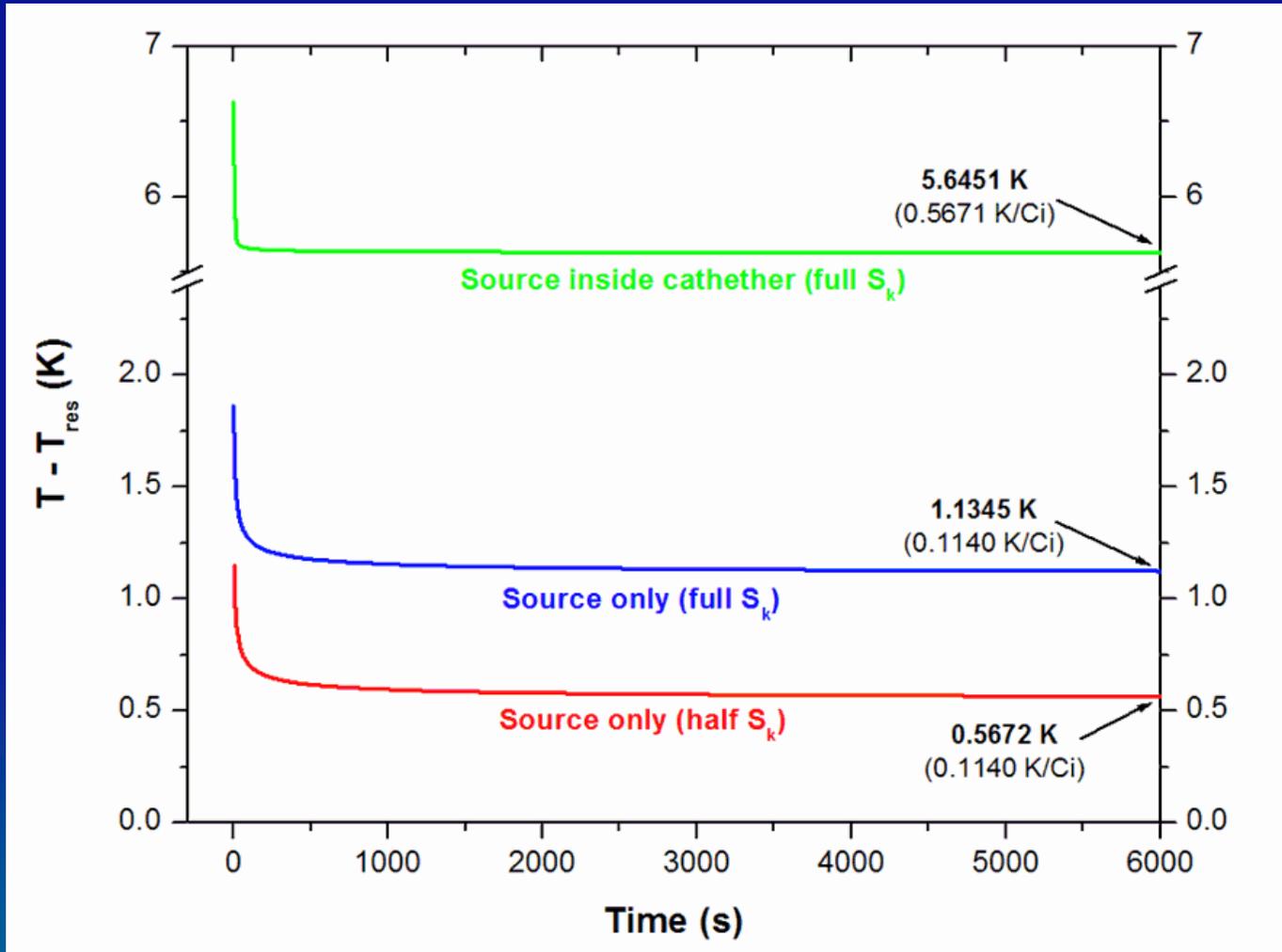


G. M. Daskalov, E. Loffler, and J. F. Williamson, "Monte Carlo-aided dosimetry of a new high dose-rate brachytherapy source," *Med. Phys.* 25, 2200 (1998).

# Position Uncertainty



# Source Self-Heating



# Generic Equation

$$D_w = c_{w, const P} g \Delta T g \prod k$$

$k_{hd}$  = correction for the heat defect (chemical rx in water)

$k_{ht}$  = correction for the heat transfer

$k_p$  = perturbation correction (non-water materials)

$k_{dd}$  = profile correction factor (non-uniformity of dose profile)

$k_\rho$  = density correction factor (difference in density between the calorimeter operation temp and the temp at which another detector, exp. ion chamber, is calibrated)