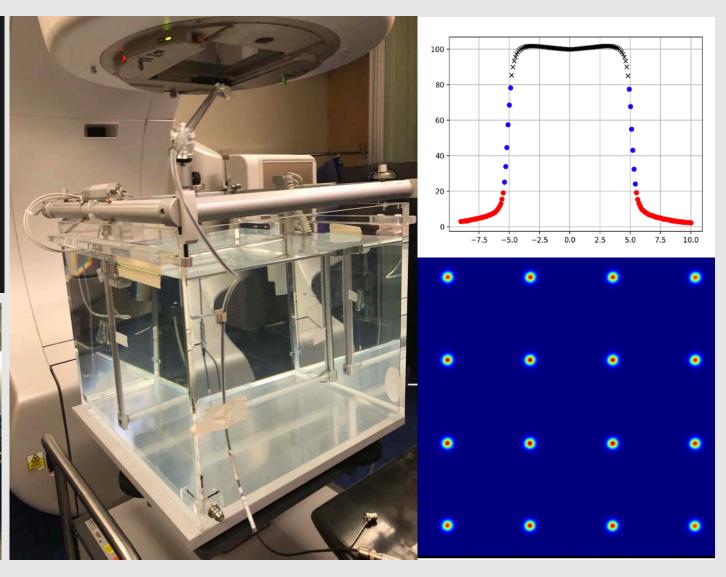
Radiation Dose: External Beam Radiation Therapy Conventions and the Evolving Field of Radiopharmaceutical Therapy

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Disclosures

- % of 2340 cGy 105 100 95_ 90 64. 43_ 30_ 10

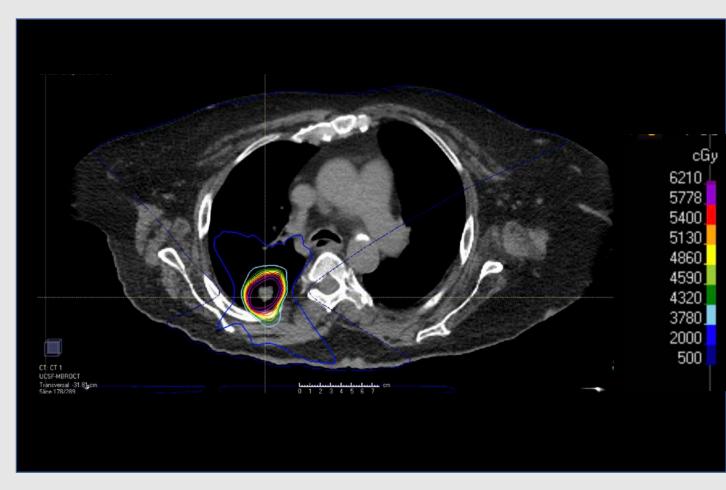
- No financial disclosures
- I work in therapeutic medical physics



External Beam Radiation Therapy

 In external beam therapy, patients receive a conformal radiation dose to targets, while healthy structures receive minimal radiation dose.

- Every treatment plan is designed for the individual patient. Most patients treatment plans are based upon CT and/or MR images.
- Patient setup is highly reproducible; most patients are setup with daily xray images and/or CBCT images.

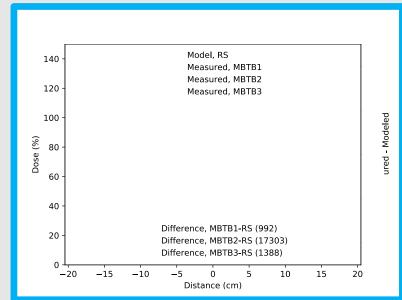


An example of a patient treatment plan

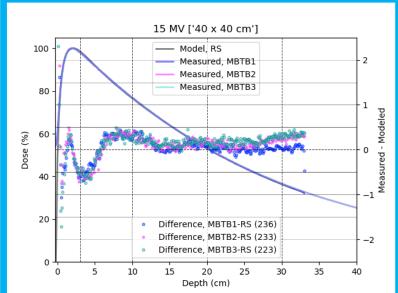


Commissioning of Linear Accelerators

- Before a linear accelerator is used for clinical treatments it is fully characterized.
- A complex beam model is created in the treatment planning system (TPS)
- The beam model is validated by creating many treatment plans that test the system, and measuring the dose (point or 3D measurements)









Output Calibrations: TG-51

After characterizing the radiation produced by the linac, physicists will calibrate the output so that a known number of monitor units produce a known amount of radiation:

e.g. 100 MU = 100 cGy for a 10 cm X 10 cm field at 100 cm SSD at a depth of dmax.

AAPM's TG-51 protocol for clinical reference dosimetry of high-energy photon and electron beams

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\mathbf{T}	G-51 Worksheet A: Photon Beams	
1	. Site data Institution: Physicist: Date: Accel or 60 Co Mfr: Model & Serial number:	
2	Nominal photon energy/beam identifier:MV Instrumentation a. Chamber model: Serial number:	
	cavity inner radius ($r_{\rm cav}$, Table III): cm Waterproof: yes no cm If no, is waterproofing ≤ 1 mm PMMA or thin latex?: yes no b. Electrometer model: Serial number:	
\ \ \ \ \ \ \ \ \ \ \ \ \ \ \ \ \ \ \	i. P_{elec} , electrom. corr factor(Sec.VII.B):	
	c. Calibration Factor $N_{D,w}^{60}$ (Sec.V):Gy/C (or Gy/rdg) Date of report (not to exceed 2 years):	
3	B. Measurement Conditions (10×10cm², point of measurement at 10 cm depth (water equivalent a. Distance (SSD or SAD): b. Field size: on surface(SSD setup): at detector(SAD setup):	
	c. Number of monitor units: MU (min for ⁶⁰ Co)	
4	4. Beam Quality (Sec.VIII.B –not needed for ⁶⁰ Co) If energy < 10 MV, use no lead foil. Measure %dd(10) 1% denth-dose at 10 cm denth for curve shifted upstream by 0.6 r. 1	

Measure $\%dd(10)$ [% depth-dose at 10 cm depth for curve shifted upstream by 0.6 $r_{ m cav}$]
Field size 10×10cm ² on surface,SSD=100 cm: yes no
a. $\%dd(10)_x = \%dd(10)$
If energy ≥ 10 MV
Distance of 1 mm lead foil from phantom surface 50 ± 5 cm 30 ± 1 cm
Measure $\%dd(10)_{ m Pb}$ [% depth-dose at 10 cm depth for curve shifted upstream by 0.6 $r_{ m ca}$
Field size 10×10cm ² on surface,SSD=100 cm: yes no
$%dd(10)_{\sf Pb}$ (includes e $^-$ contamination):

Eq.(13)

 $[\%dd(10)_{Pb} \ge 73\%]$

 $[\%dd(10)_{Pb} \ge 71\%]$

 $%dd(10)_x = %dd(10)_{Pb}$

yes no

50 cm: $%dd(10)_x = [0.8905 + 0.00150\%dd(10)_{Pb}]\%dd(10)_{Pb}$

30 cm: $%dd(10)_x = [0.8116 + 0.00264\%dd(10)_{Pb}] %dd(10)_{Pb}$

If $\%dd(10)_{Pb} < 71\%$ (30cm) or 73%(50cm):

b. $\%dd(10)_x$ (for open beam):

Has lead foil been removed?

External Validation: IROC OSLDs

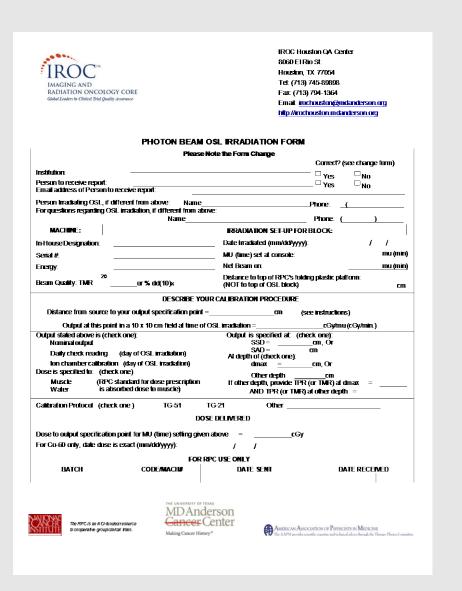
Institutions can verify the calibration by irradiating small phantoms with TLDs or OSLDs inserted in them

A known radiation dose is delivered and the phantoms are returned to IROC.

The received radiation dose is externally verified by IROC

Listed below are the results for the TLD irradiated June 26, 2014 on the Mobetron s/n 49:

Electron Energy TLD Ratio – MDACC/INST (difference in mm between TLD depth and Inst depth)
6 MeV 1.00 (-1 mm)
9 MeV 1.00 (0 mm)
12 MeV 1.00 (0 mm)



In addition ...

- To participate in clinical trials, end-toend testing is also required.
- Phantoms with TLDs are shipped to the institution where they are imaged and a treatment plan is created and delivered.
- The phantoms are then shipped back to IROC, where the radiation dose delivered to the TLDs is determined.
- The credentialing process ensures that participating sites are capable of delivering complex radiation treatment plans as intended

Report of Lung Phantom Irradiation

Date of Report: January 6, 2017

Institution: University of California - San Francisco

Physicist: Joey Cheung

Radiation Machine: Varian, TrueBeam (1737) – 6 MV

Collimator: MLC

Technique: IMRT - VMAT

Treatment Planning System: Philips, Pinnacle (3D/IMRT) – Collapsed Cone Convolution

Date of Irradiation: November 18, 2016

Description of procedure:

An anthropomorphic lung phantom incorporating a cylindrical dosimetry insert that simulated the left lung was placed in the supine position in a CT scanner and imaged. The insert contained a spherical centered target. TLD capsules located near the center of the target provided point dose information and three sheets of GAFChromic™ Dosimetry Media provided dose distributions in the axial, coronal and sagittal planes. The phantom included heart and spinal cord structures, each one containing one TLD capsule. The right lung was also included. The phantom with the insert was irradiated to approximately 6 Gy using a IMRT technique. The analyses of the results were based on dose calculation applying correction for tissue heterogeneity.

The dosimetric precision of the TLD is 3%, and the spatial precision of the film and densitometer system is 1 mm.

Summary of TLD and film results:

Location	IROC-H vs. Inst.	Criteria	Acceptable
PTV_TLD_sup	0.97	0.92 – 1.05	Yes
PTV_TLD_inf	0.98	0.92 - 1.05	Yes

Film Plane	Gamma Index*	Criteria	Acceptable
Axial	96%	≥ 80%	Yes
Coronal	95%	≥ 80%	Yes
Sagittal	92%	≥ 80%	Yes
Average over 3 planes	94%	≥ 85%	Yes

^{*}Percentage of points meeting gamma-index criteria of 7% and 5 mm

The phantom irradiation results listed in the table above **do meet** the criteria established by the IROC Houston in collaboration with the cooperative study groups. Therefore, your institution **has satisfied** the phantom irradiation component of the credentialing process to enter patients onto clinical trials.

TLD and Film Analysis by: Paige Taylor, M.S. and Hunter Mehrens

Report Checked by:

David S. Followill, Ph D.

Director, IROC Houston QA Center

Daily, Monthly and Annual QA

- In addition to the calibration described, routine QA is performed on linacs to ensure dose constancy.
- This includes daily QA, monthly QA and performing TG-51 annually
- IROC OSLDs are irradiated annually.
- For complex treatments (e.g. IMRT), patient specific QA is also performed before the patient receives treatment

Table I. Daily.			
	Machine-type tolerance		
Procedure	Non-IMRT	IMRT	SRS/SBRT
Dosimetry			
X-ray output constancy (all energies) Electron output constancy (weekly, except for machines with unique e-monitoring requiring daily)		3%	

Task Group 142 report: Quality assurance of medical accelerators^{a)}

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Todd Holmes

Varian Medical Systems, Palo Alto, California

Training physicists in external beam RT

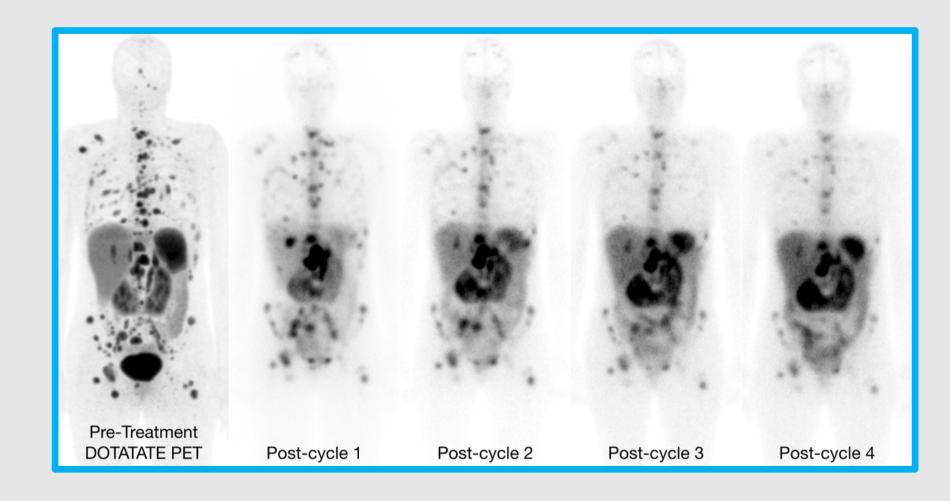
 Board certification by the ABR in therapeutic radiation physics requires a CAMPEP accredited residency

 Residents have many opportunities to learn how accelerators are calibrated and how routine QA is performed



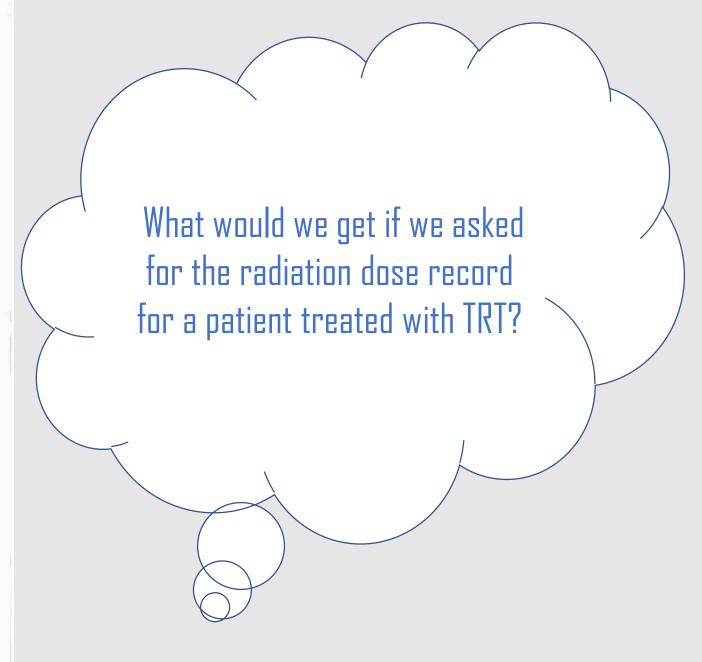
Part 2: Radionuclide Therapy

¹⁷⁷Lu-DOTATATE



UCSF Therapeutic Lu-177 Lutathera Dispensing Checklist

LUTATHERA ARRIVAL	
Date Arrived: Lot Number:	LT 170502 A-03 24.9.
DOSE Nuc Med I	nitials: Rad Safety Initials: BH
	MRN:
Planned Le Color Date LANCE. The Date of the Party of the	
Planned Infusion Date: Planned Infusion Time Dispensed Activity: Planned Infusion Time	e:
100 0	_mCi
INFUSION RECORD	
1. Start Time: 2. Find Time (end of Second flush): 3. Residual Activity: 4. Total Activity Infused: 5. Actual Treatment Dose: 6. mRem/hr at 1 meter at end of first flush: 7. mRem/hr at 1 meter at discharge:	8
ATTENDING DOSE SIGN-OFF (REQUIRED PRIOR TO INF	USION START)
Dispensed Activity to be Infused: 188 · 6 mCi	Myc-Med White Med White Med White Med White Med
Final Signatures Approving Infusion of Dispensed Activity:	



¹⁷⁷LU-DOTATATE PHASE 3 TRIAL IN MIDGUT NEUROENDOCRINE TUMORS

SUPPLEMENTARY APPENDIX

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Supplementary Figure 2. Relative Change from Baseline in (c) Neutrophil Count
Supplementary Figure 2. Relative Change from Baseline in (d) Platelet Count
Supplementary Figure 3. Creatinine Clearance Over Time in the Study

Supplementary Table S2. 177Lu-DOTATATE Exposure.*

Patients who completed treatment phase (N=103†)	no. (%)
Number of administrations	
4	79 (77)
3	6 (6)
2	12 (12)
1	5 (5)
0	1 (1)
All treated patients (N=111)	
No DMT	103 (93)
DMT	8 (7)

^{*} DMT denotes dose-modifying toxicity.

Phase 3 Trial of ¹⁷⁷Lu-Dotatate for Midgut Neuroendocrine Tumors

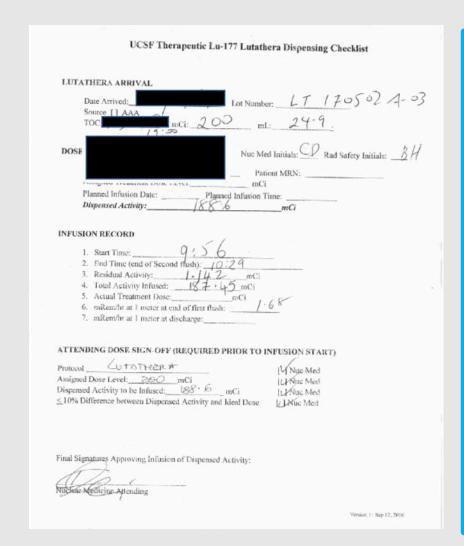
J. Strosberg, G. El-Haddad, E. Wolin, A. Hendifar, J. Yao, B. Chasen, E. Mittra, P.L. Kunz, M.H. Kulke, H. Jacene, D. Bushnell, T.M. O'Dorisio, R.P. Baum, H.R. Kulkarni, M. Caplin, R. Lebtahi, T. Hobday, E. Delpassand, E. Van Cutsem, A. Benson, R. Srirajaskanthan, M. Pavel, J. Mora, J. Berlin, E. Grande, N. Reed, E. Seregni, K. Öberg, M. Lopera Sierra, P. Santoro, T. Thevenet, J.L. Erion, P. Ruszniewski, D. Kwekkeboom, and E. Krenning, for the NETTER-1 Trial Investigators*

[†] Excluding patients still under treatment (n=8) or no treatment (n = 5).

24 hour post-administration SPECT/CT

All patients treated with Lu-177 DOTATATE at UCSF have a 24 hour post-administration SPECT/CT scan

These scans are used qualitatively



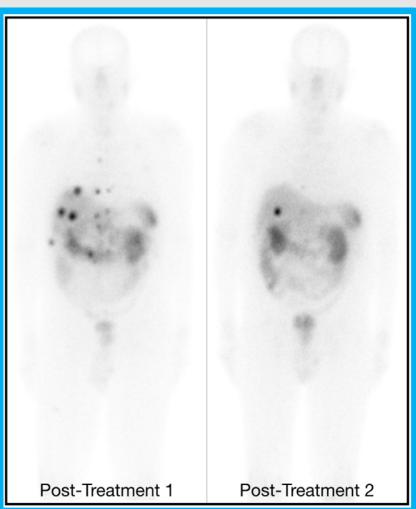


Image courtesy of Dr. Thomas Hope, UCSF Department of Radiology

Beyond Administered Activity...

- To report patient dose in Gy requires several additional steps
 - Calibrated SPECT/CT or PET/CT scanner
 - Validated dose calculation algorithm

 Recording the dose in a standardized format (e.g. RTDose)

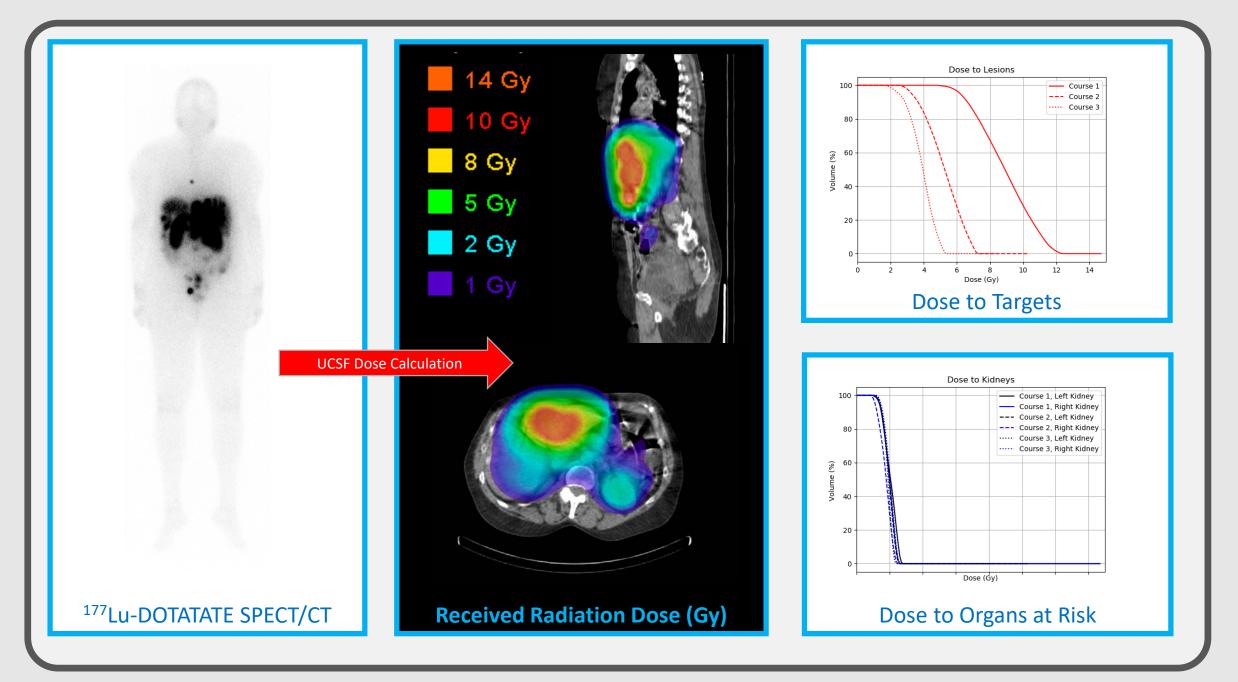
SPECIAL CONTRIBUTIONS

MIRD Pamphlet No. 26: Joint EANM/MIRD Guidelines for Quantitative ¹⁷⁷Lu SPECT Applied for Dosimetry of Radiopharmaceutical Therapy

Michael Ljungberg¹, Anna Celler², Mark W. Konijnenberg³, Keith F. Eckerman⁴, Yuni K. Dewaraja⁵, and Katarina Sjögreen-Gleisner¹

In collaboration with the SNMMI MIRD Committee: Wesley E. Bolch, A. Bertrand Brill, Frederic Fahey, Darrell R. Fisher, Robert Hobbs, Roger W. Howell, Ruby F. Meredith, George Sgouros, and Pat Zanzonico, and the EANM Dosimetry Committee: Klaus Bacher, Carlo Chiesa, Glenn Flux, Michael Lassmann, Lidia Strigari, and Stephan Walrand.





Work done in collaboration with Dr. Thomas Hope, UCSF Department of Radiology

External Beam RT

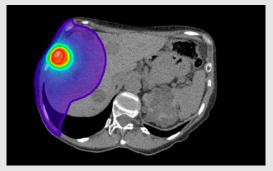
Standardized Calibration Procedures

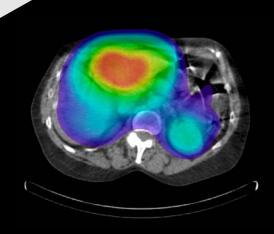
External Dose Validation Methods (phantoms)



Training for physicists who perform calibrations

Routine QA & tolerances





Targeted Radionuclide Therapy

